

Zusammenspiel elektrischer Stimuli mit sensorischen und motorischen Neuronen oder mit Muskelfasern aus technisch physiologischer Sicht - Möglichkeiten und Grenzen

GESET, Koblenz, 2022



INTERFACING NEURONS AND MUSCLES

with Functional Electrical Stimulation / Neuromodulation

Afferent Nerves

Efferent Nerves

Muscle Fibers

Sensory Functions

Motor Functions

Afferent nerves

Direct Control

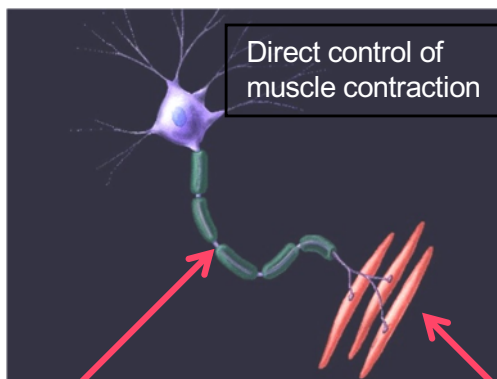
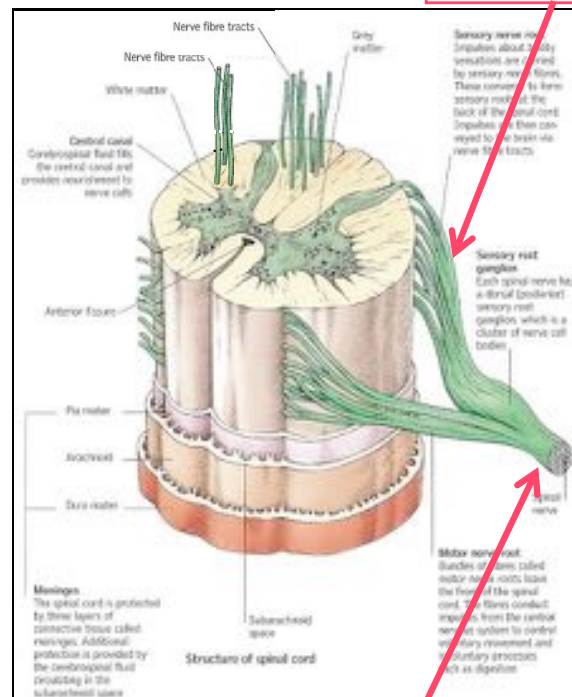
Indirect Control

Spasticity / Stiffness / Pain

Motor Control / Tissue Preservation

Conditioning, Training

Substitution of Functions

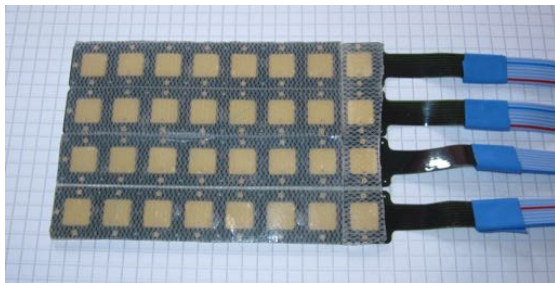


Neuromuscular - motor nerve

Denervated muscle

Mixed Nerve

Electrode-tissue interface - Shape and size of stimuli



noninvasive

Decisive and limiting
compromise on
selectivity and safety

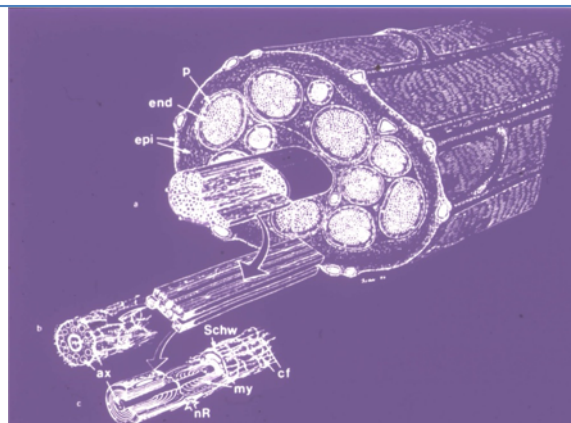
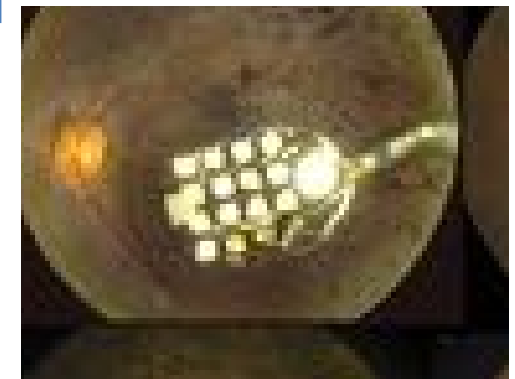
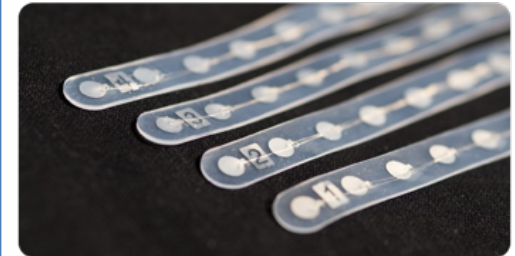
*

Generally coarse tool to
activate tiny structures

*

Integration of medical,
physiological and
engineering expertise

implanted



Electrode-tissue interface

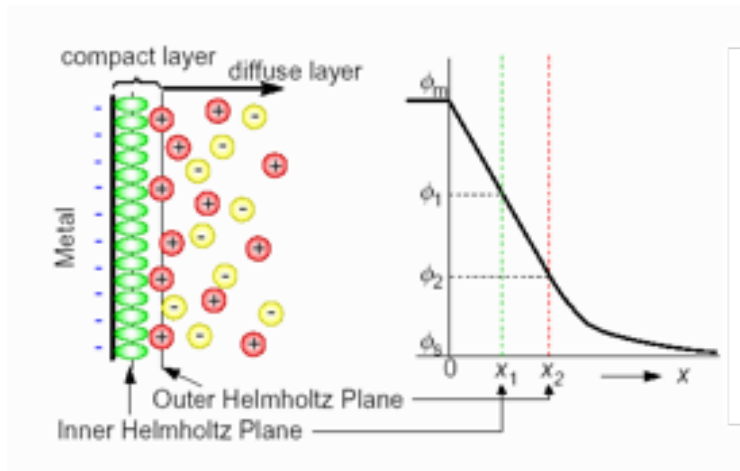
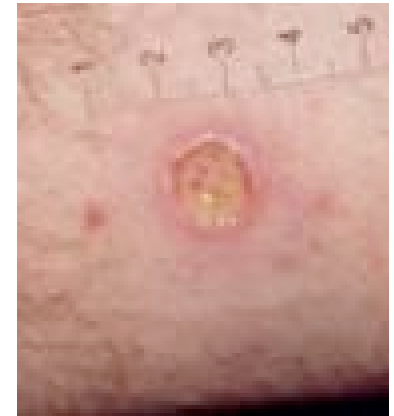
Amplitude (mA) \times Impulse width (ms) = Impulse charge (C)

- **No DC !**

positive and negative impulse phase equal

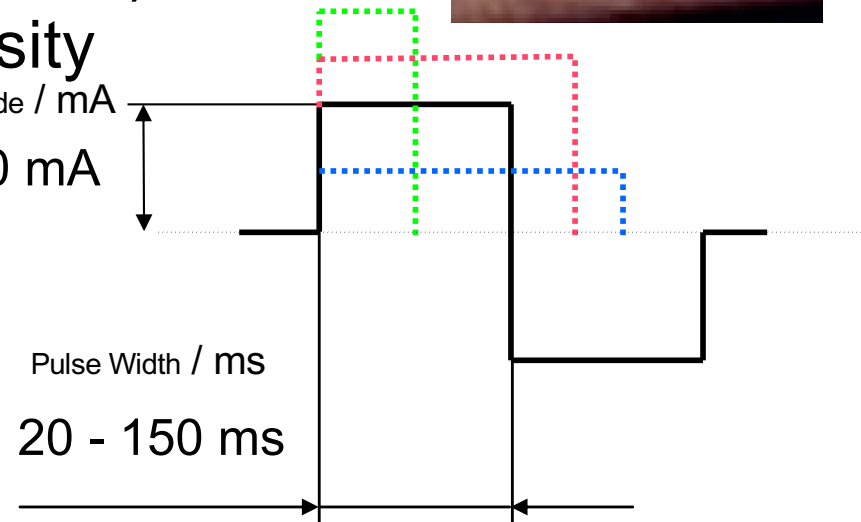
- Impulse charge / Electrode contact surface must not exceed **Charge Injection Limit** in $\mu\text{C}/\text{cm}^2$ ($\mu\text{As}/\text{cm}^2$)

- **Risk:** excessive local current density



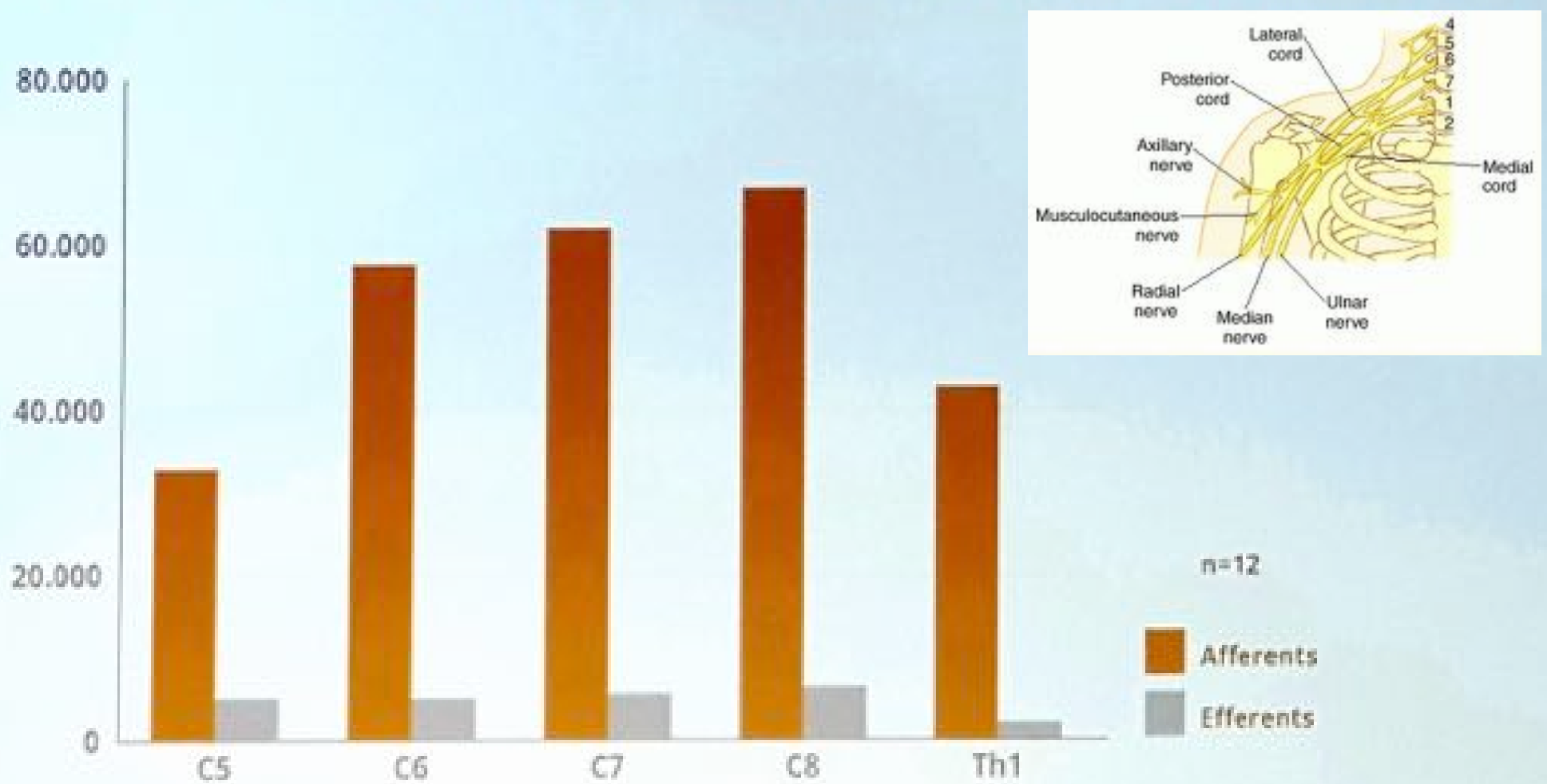
Amplitude / mA
 \Rightarrow 300 mA

Pulse Width / ms
 20 - 150 ms



Imp. charge \Rightarrow 6.000 μAs (\Rightarrow 45.000 μAs)
 200 cm^2 \Rightarrow 30 $\mu\text{C}/\text{cm}^2$ (\Rightarrow 225 $\mu\text{C}/\text{cm}^2$)

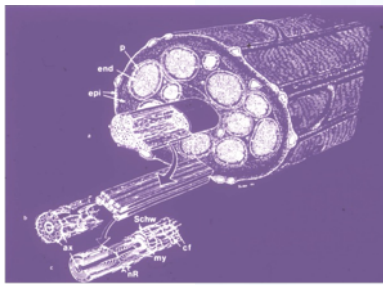
FIRST QUANTITATIVE DATA ON HUMAN BP



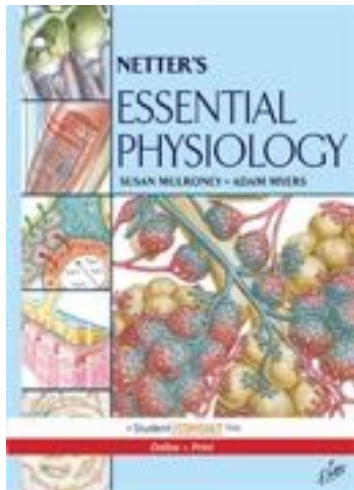
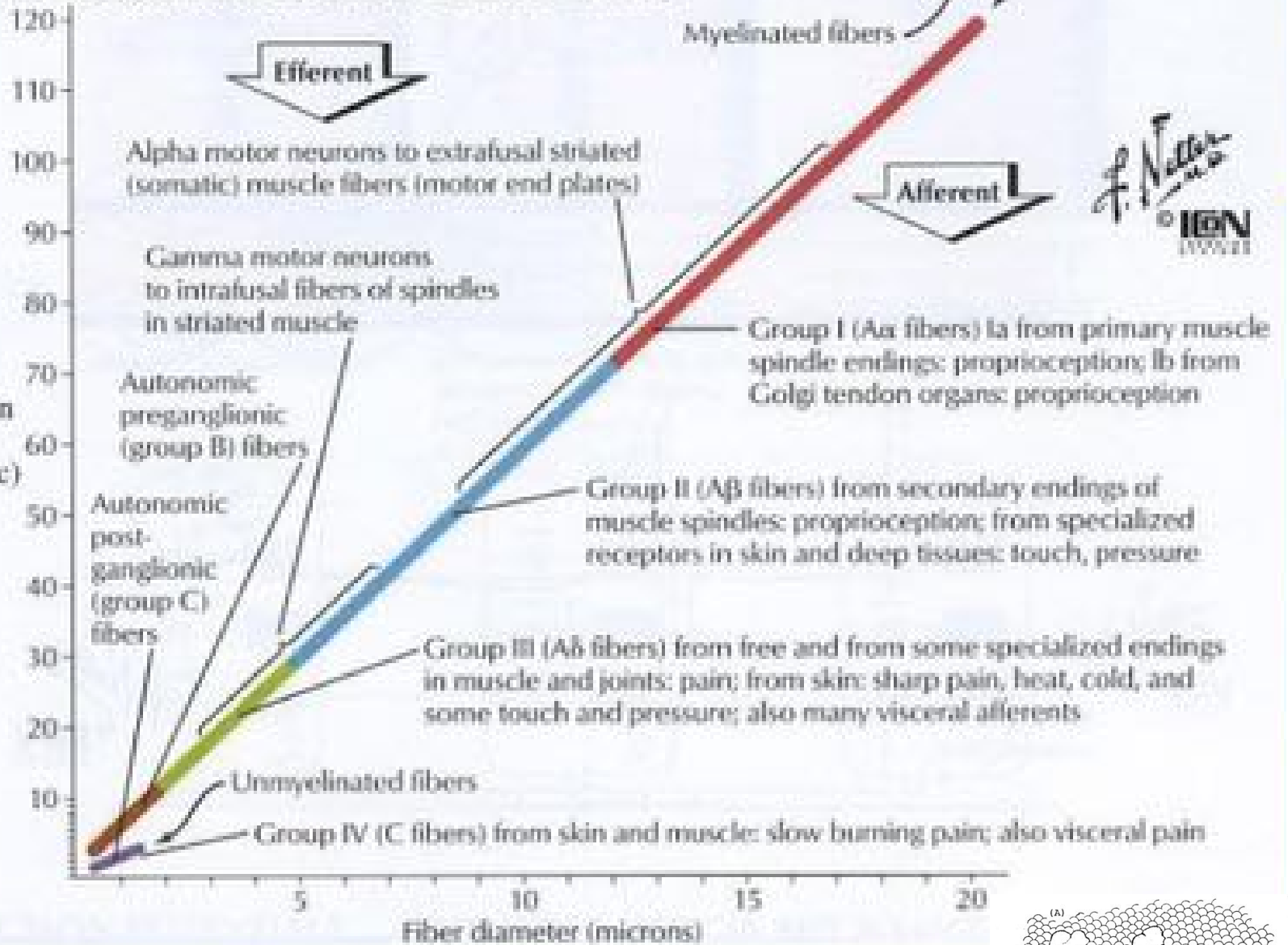
afferent – efferent
9 : 1

Gesslbauer B, et al.
Axonal components of nerves innervating the human arm.
Ann Neurol. 2017 Sep;82(3):396-408

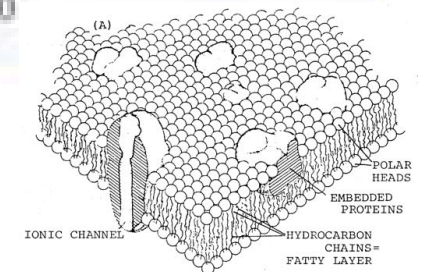
C. Classification of nerve fibers by size and conduction velocity



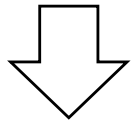
Conduction velocity (meters/sec)



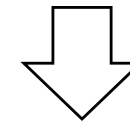
Bretscher M.S. and Raff M.C. 1975. Mammalian plasma membranes. Nature 258, 43-49



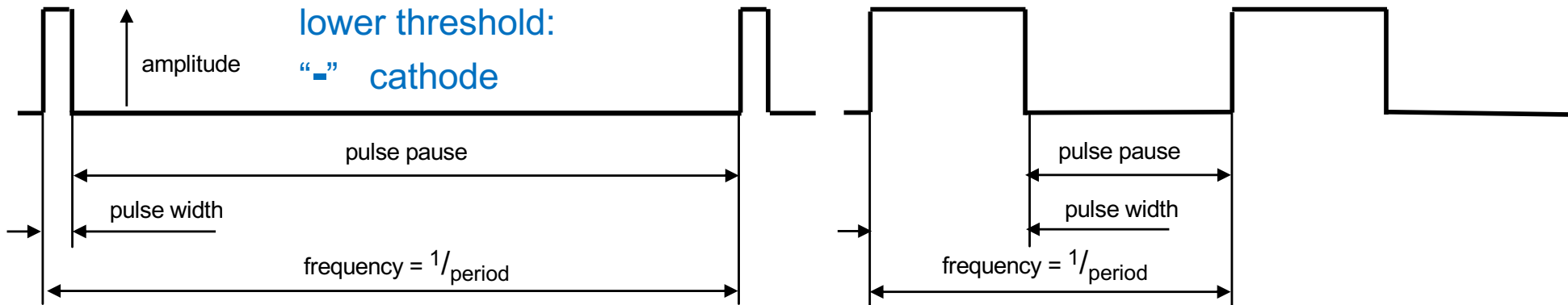
Nerve Stimulation



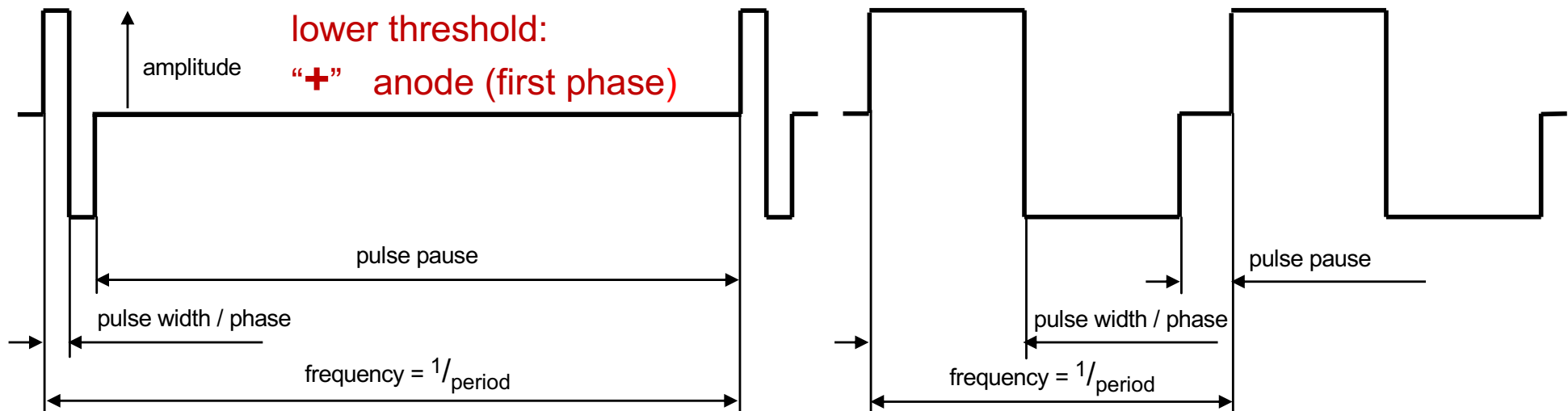
(Muscle Stimulation)

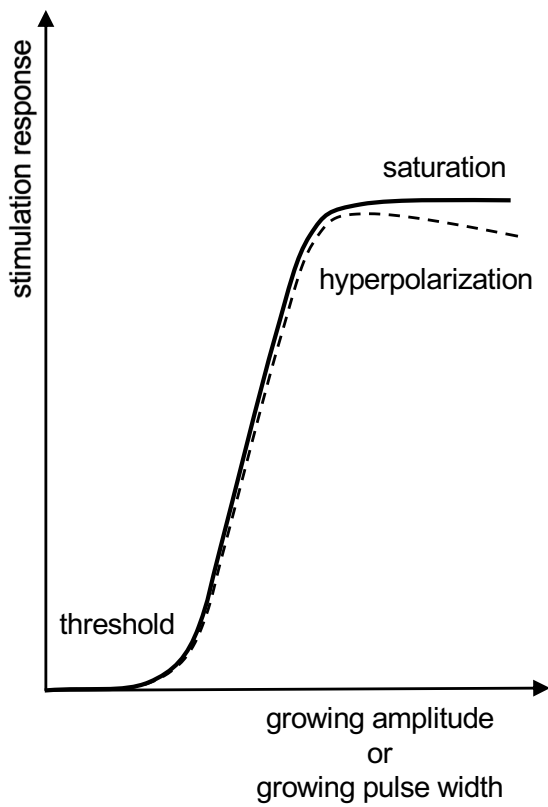


monophasic pulse shape

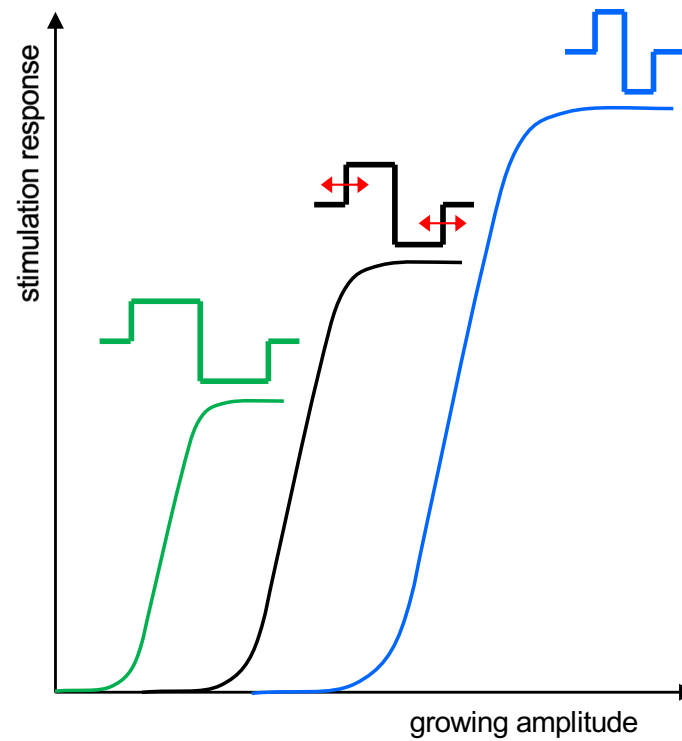


biphasic pulse shape

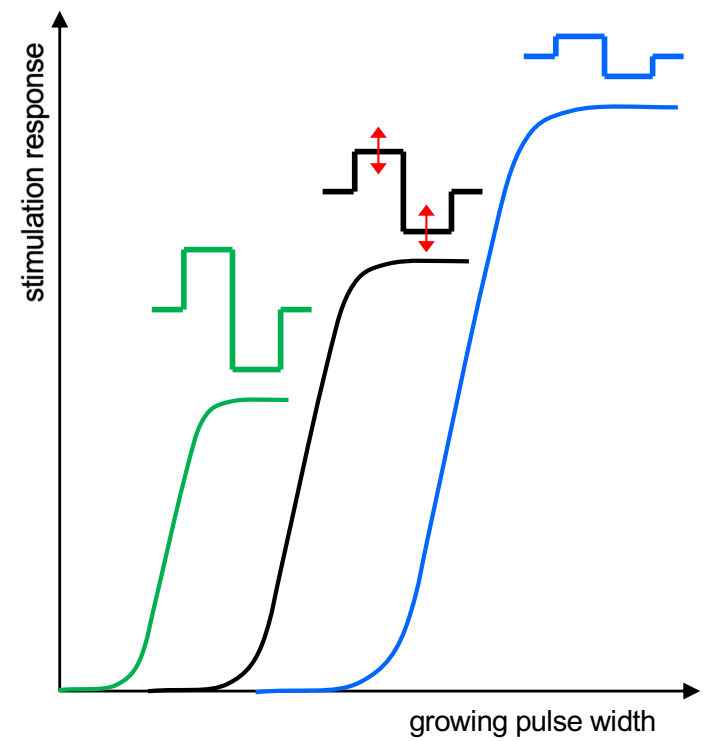




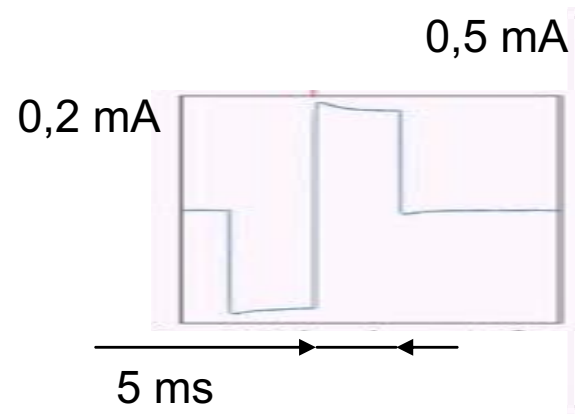
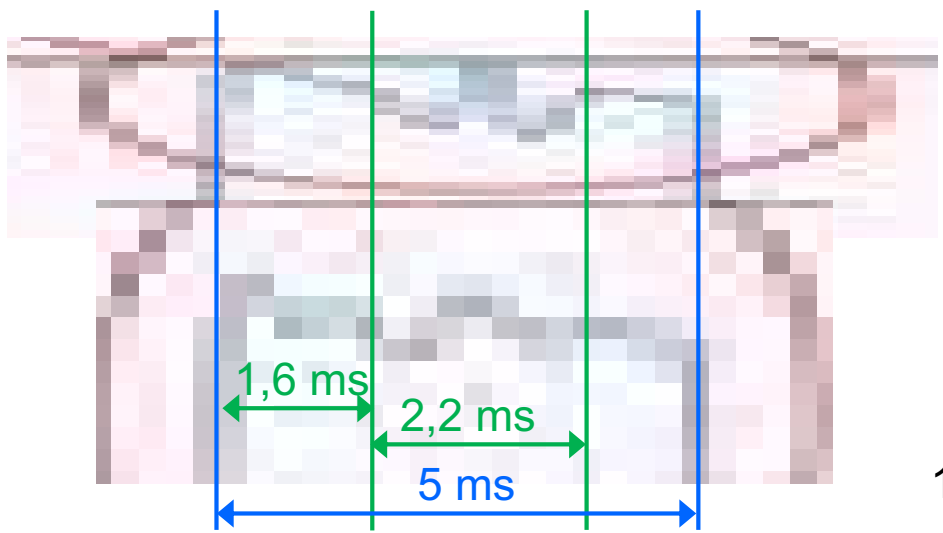
typical recruitment curve,
threshold to saturation



typical recruitment curve,
amplitude variation, constant pulse width

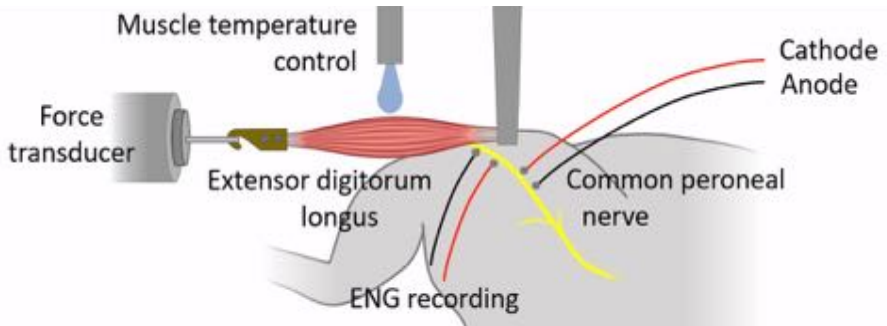
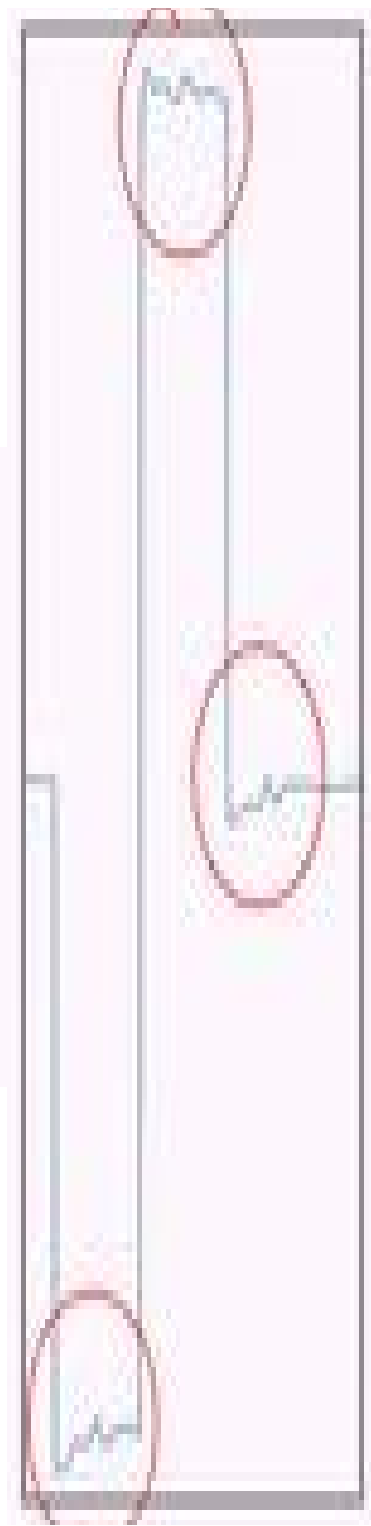


typical recruitment curve,
pulse width variation, constant amplitude

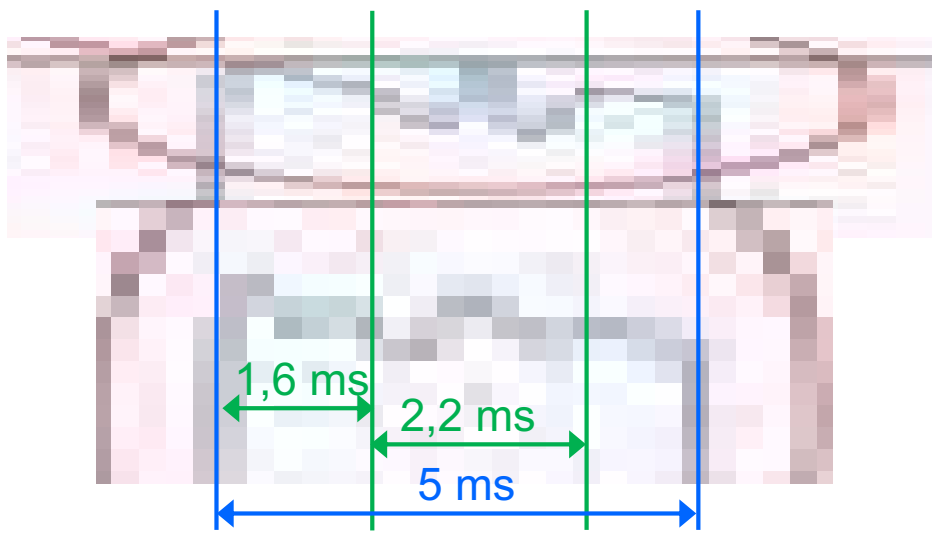


1 mA

2 mA



Steffen Eickhoff, Jonathan Jarvis – John Moores University, Liverpool
UNPUBLISHED DATA

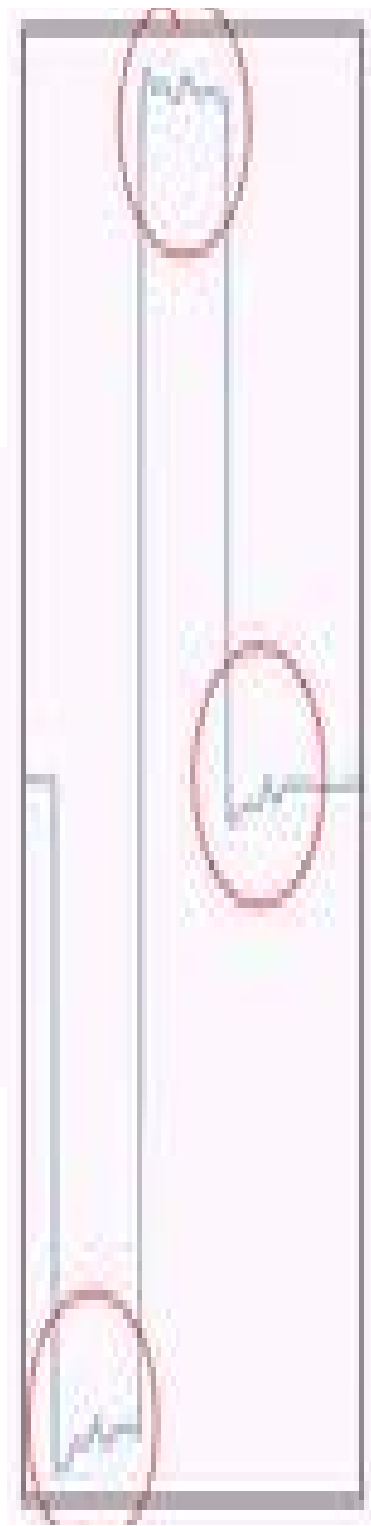
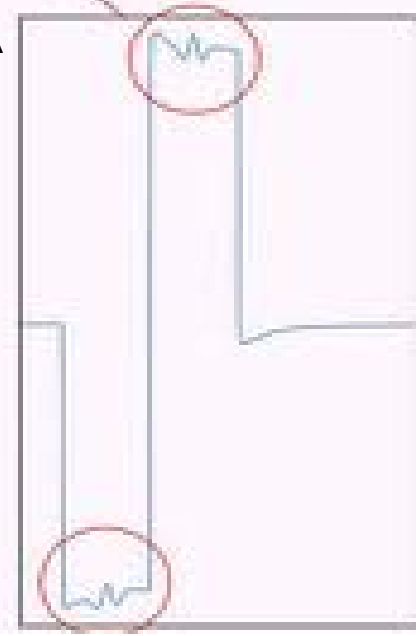
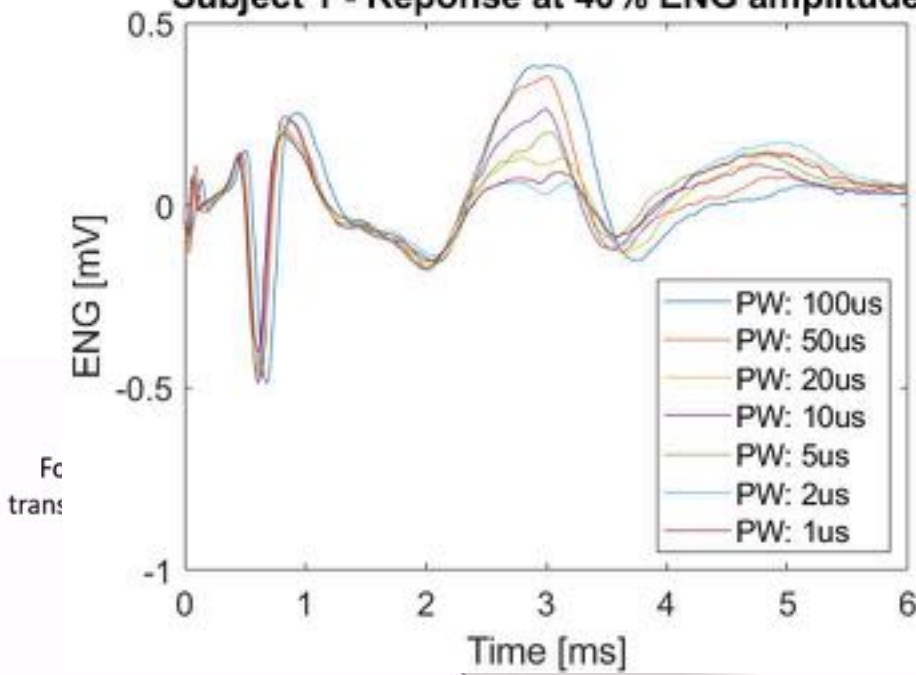


2 mA

1 mA

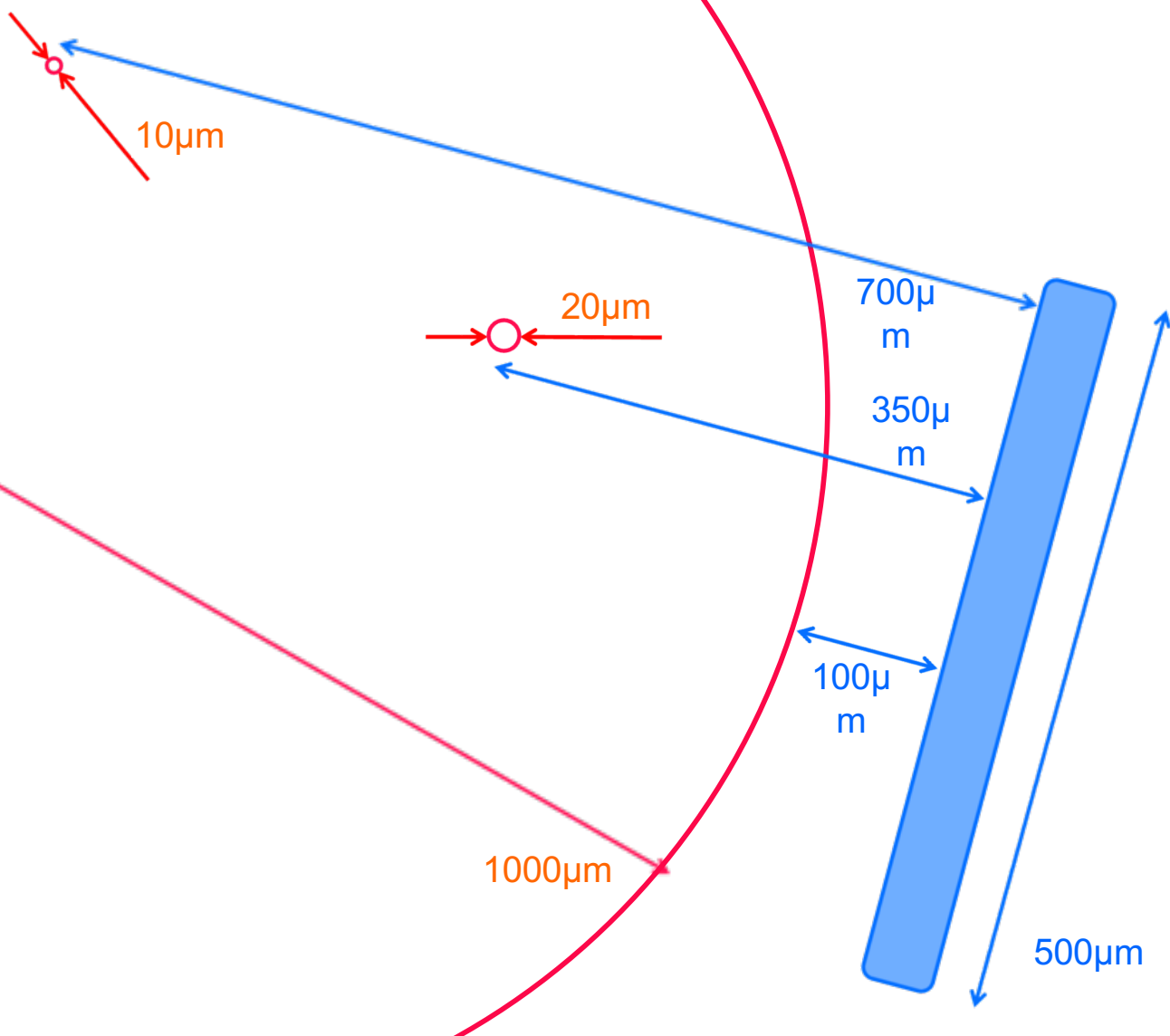
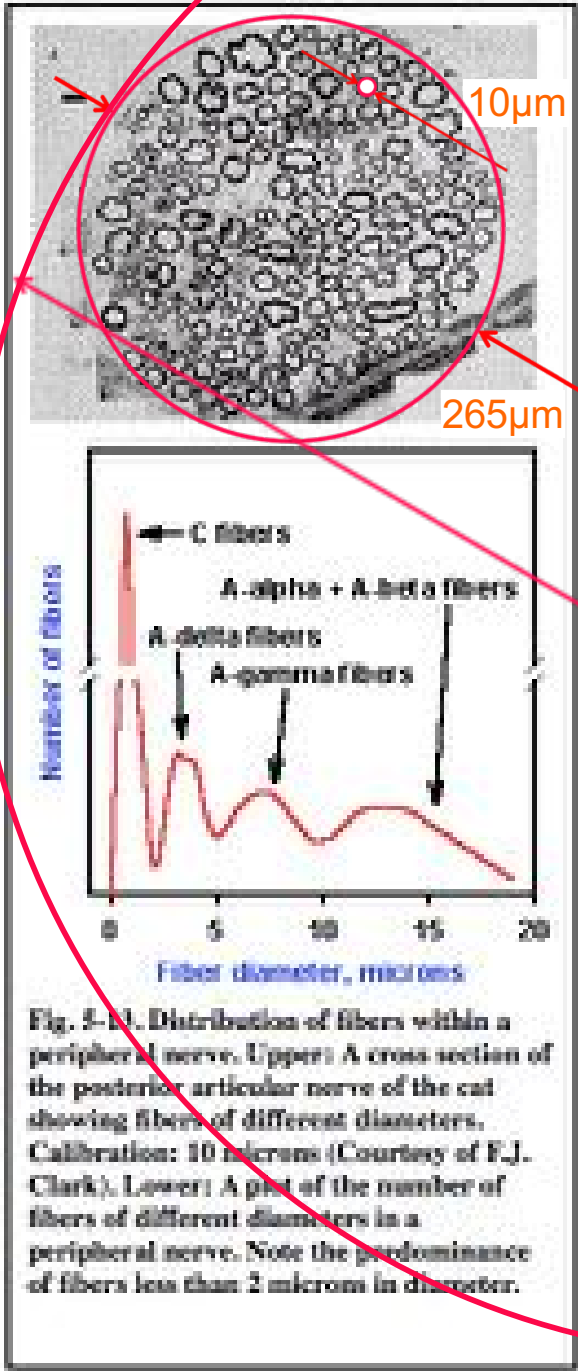
0,5 mA

Subject 1 - Reponse at 40% ENG amplitude



Johannes Proksch - Steffen Eickhoff, Jonathan Jarvis,
John Moores University, Liverpool
UNPUBLISHED DATA

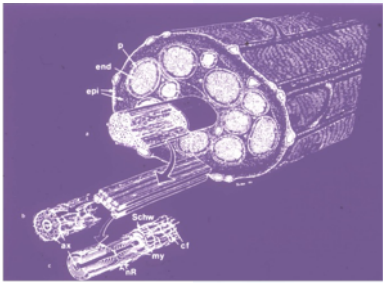
SELECTIVITY



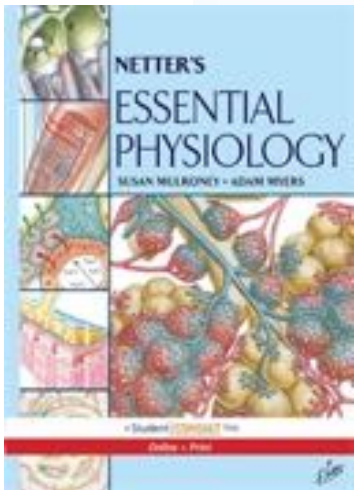
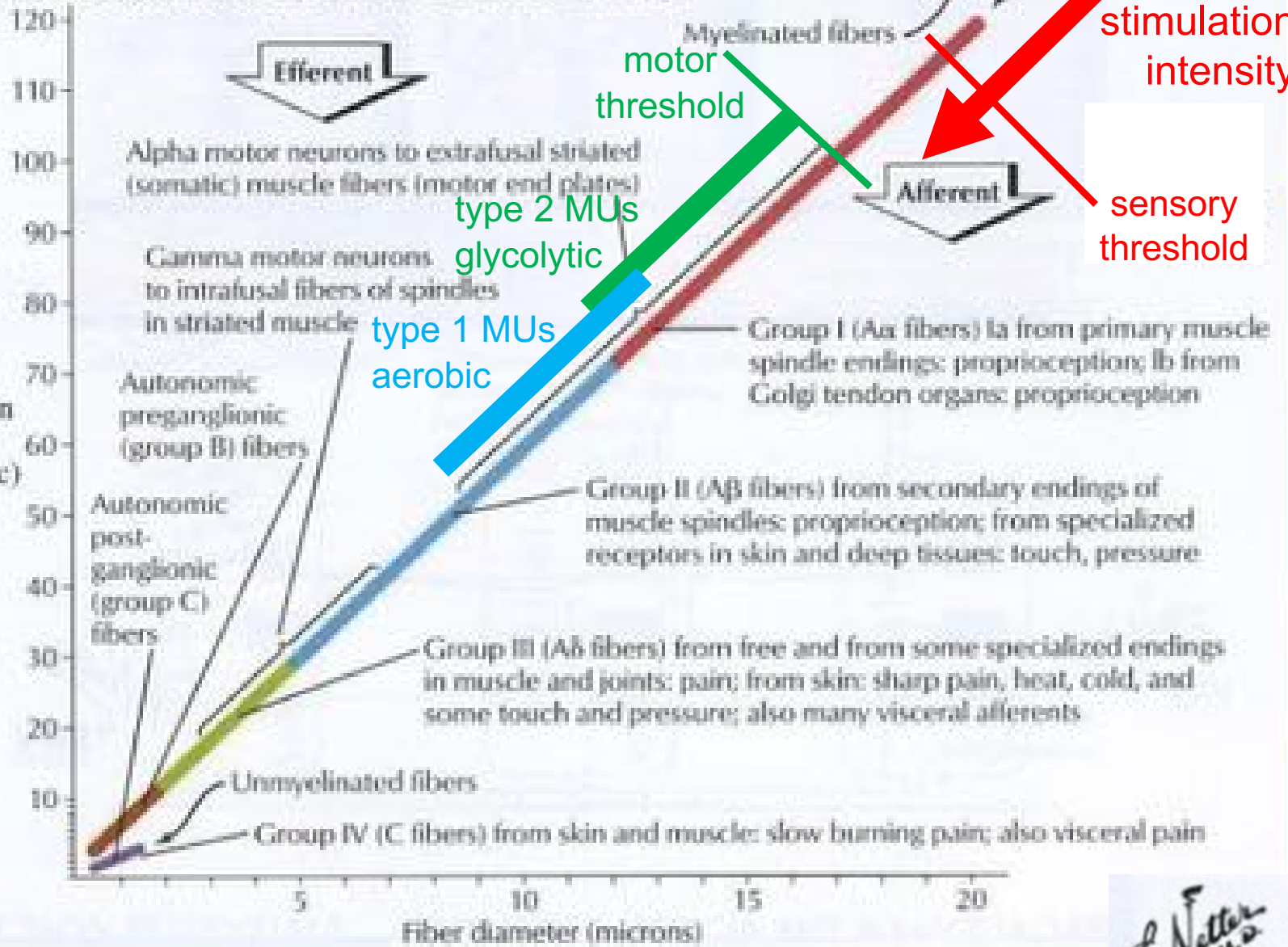
THRESHOLDS / Depolarisation / Hyperpolarisation:

- Inverse proportional fiber size
- Prop. to square of distance

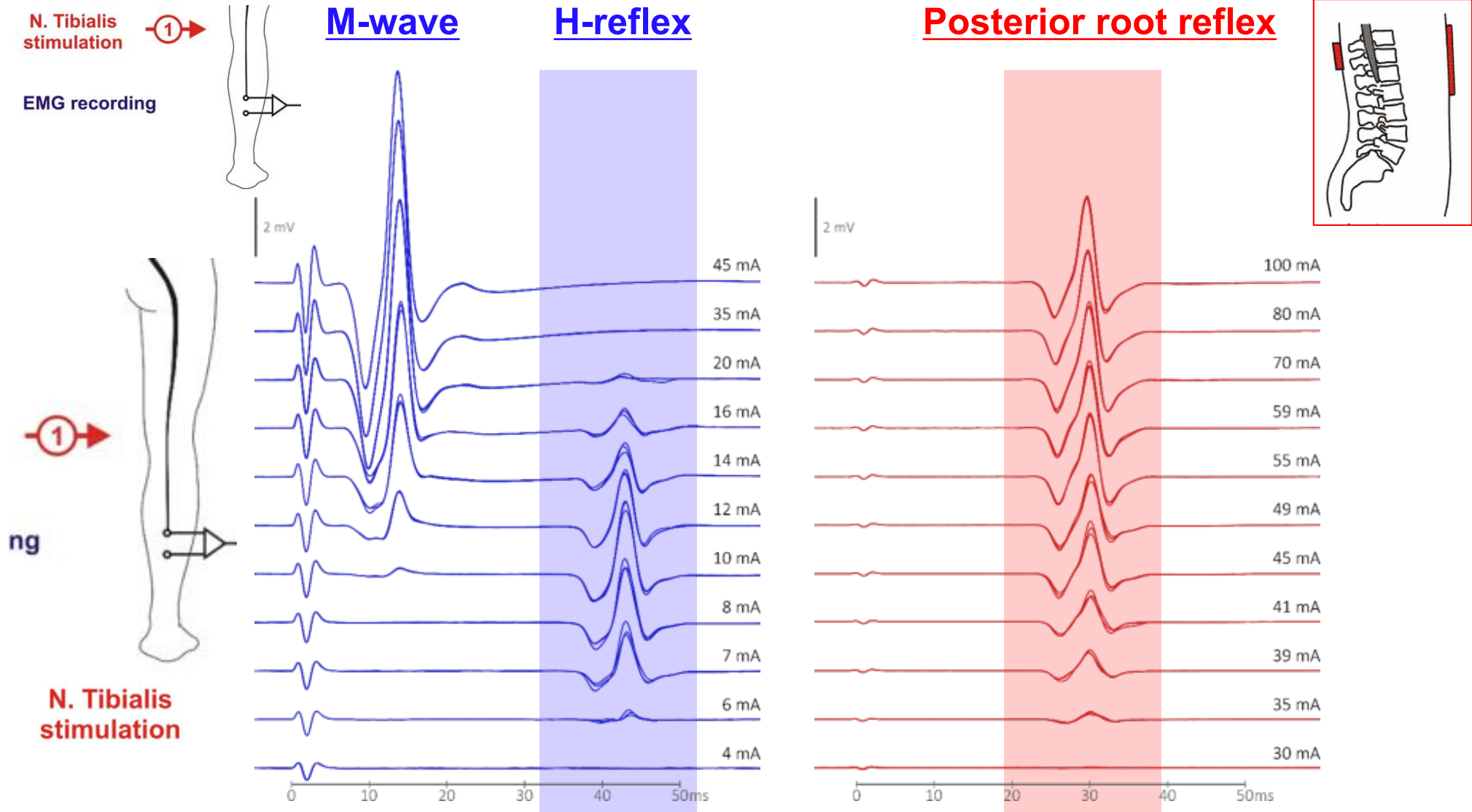
C. Classification of nerve fibers by size and conduction velocity

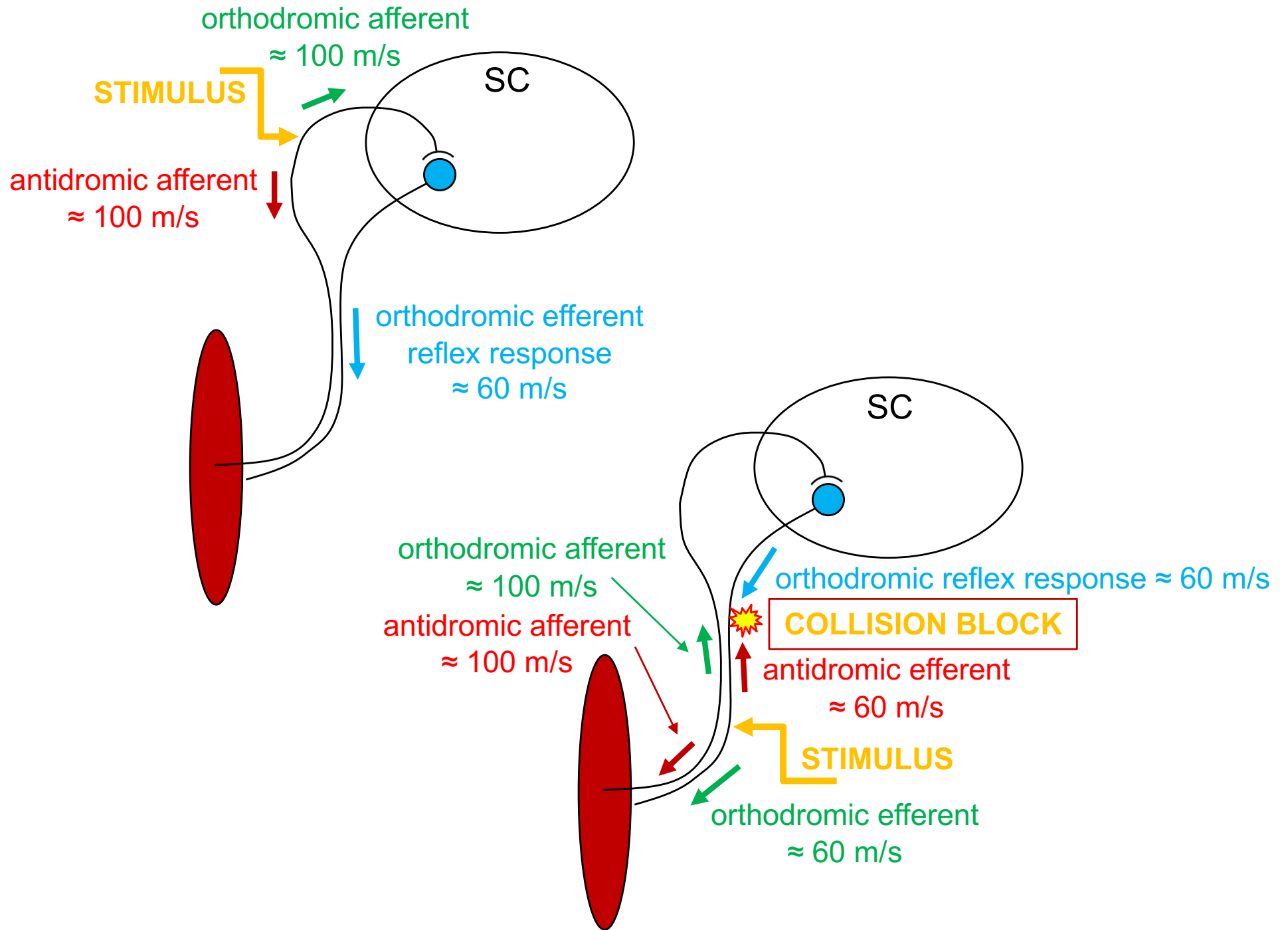


Conduction velocity (meters/sec)



H-reflex and posterior root reflex in the soleus muscle





If we have an idea on fiber recruitment –

- what about neural processing / control of movement ?

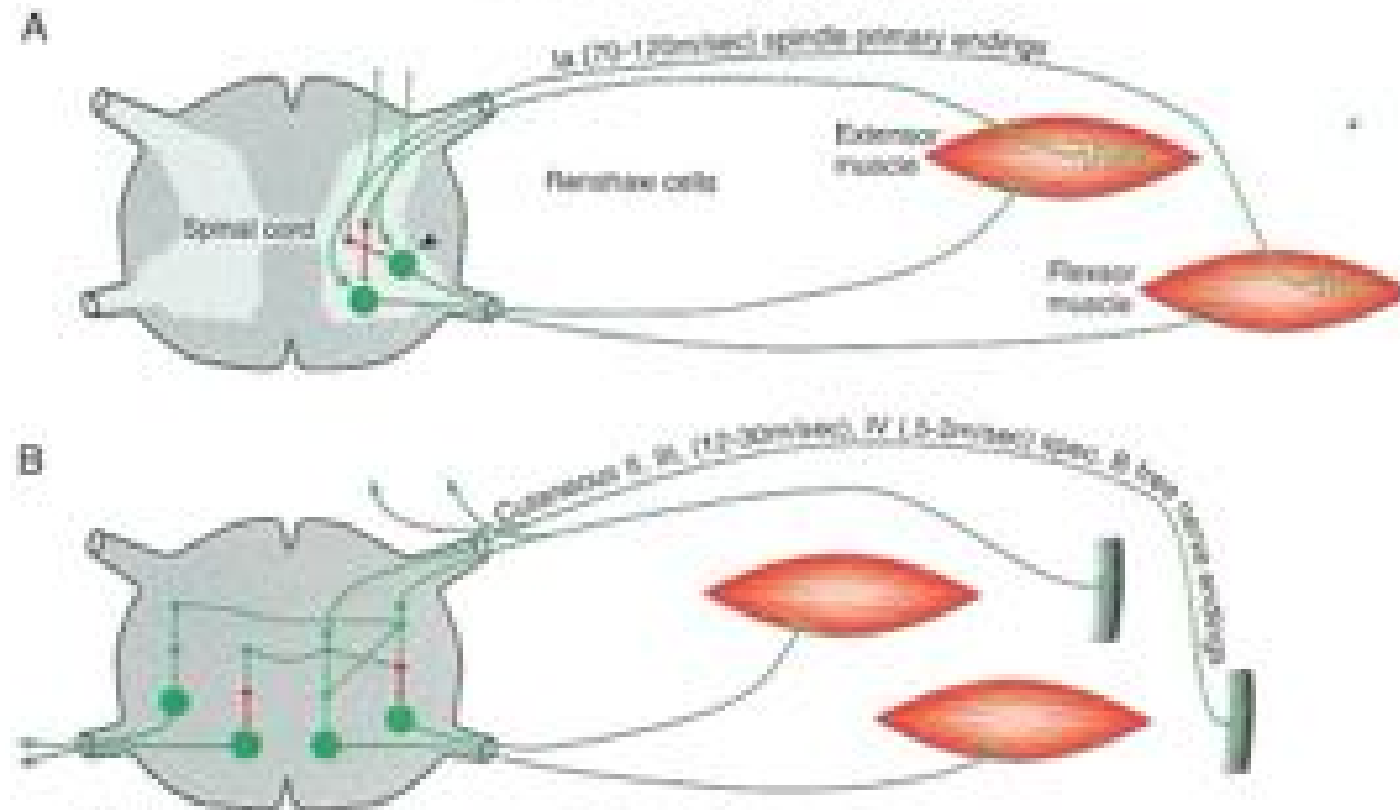
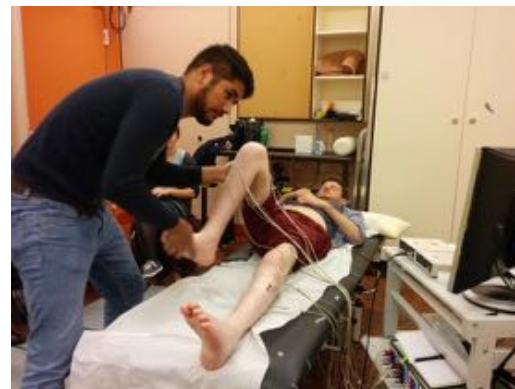
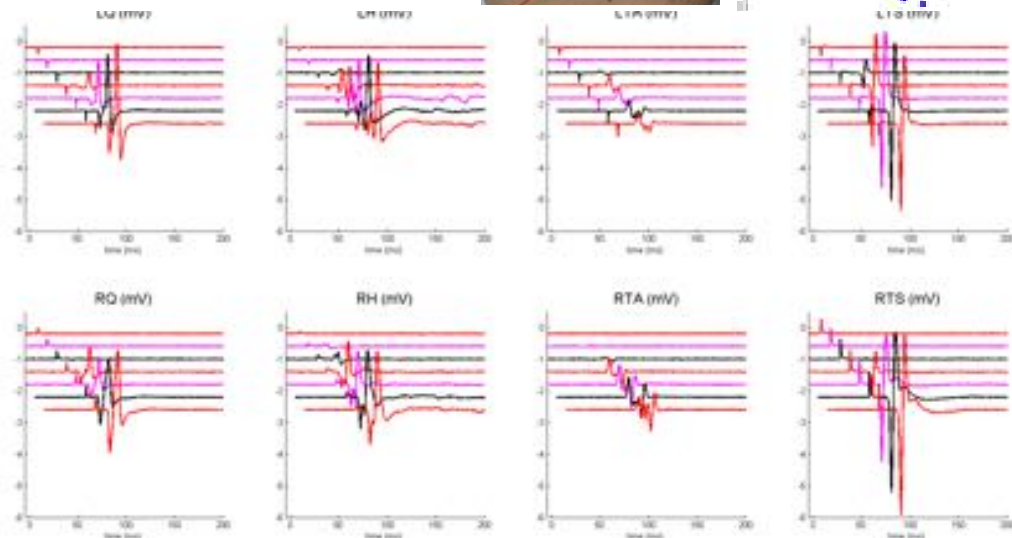
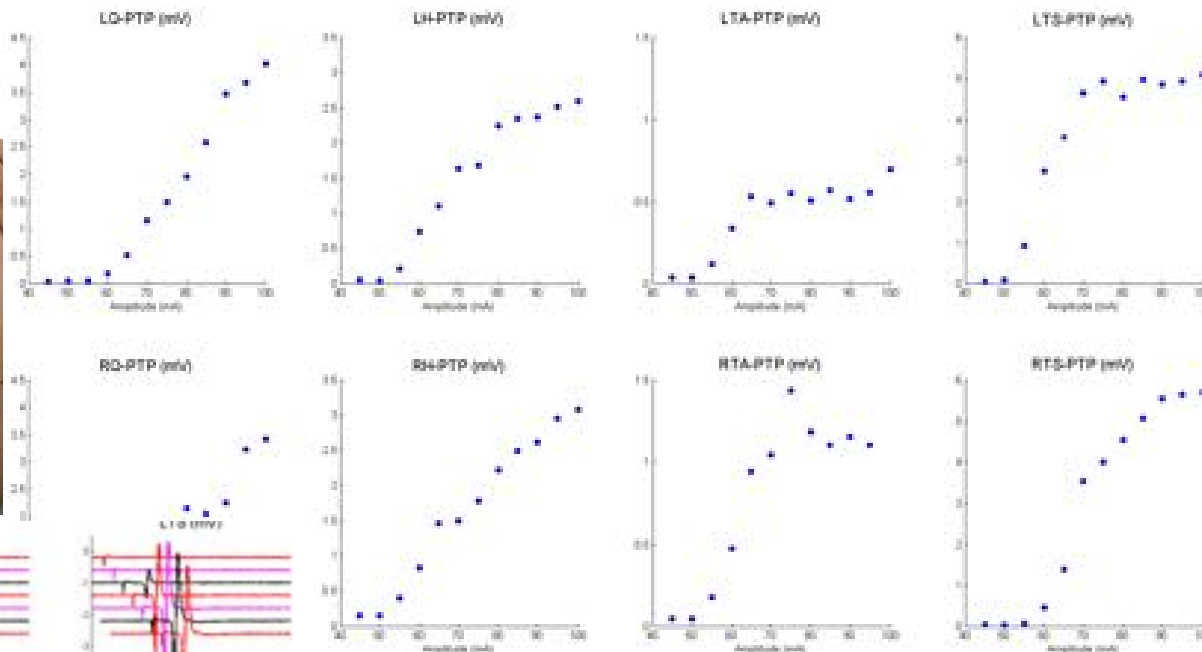
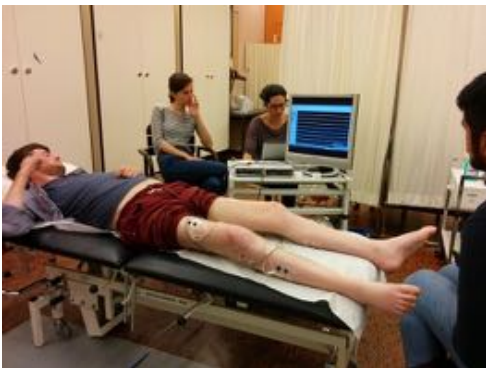


FIGURE 29.1 Circuitry for segmental spinal reflexes. Ia spindle reflexes are activated by stretch of the muscle and cause excitation of that muscle and its synergists and reciprocal inhibition of its antagonists. Skin reflexes (activated by a noxious stimulus) may cause withdrawal of the limb away from the stimulus with a supporting reaction in the opposite limb. Adapted from Eskin and Montgomery, *Neurobiology of Disease*, Oxford University Press, New York, 1990.

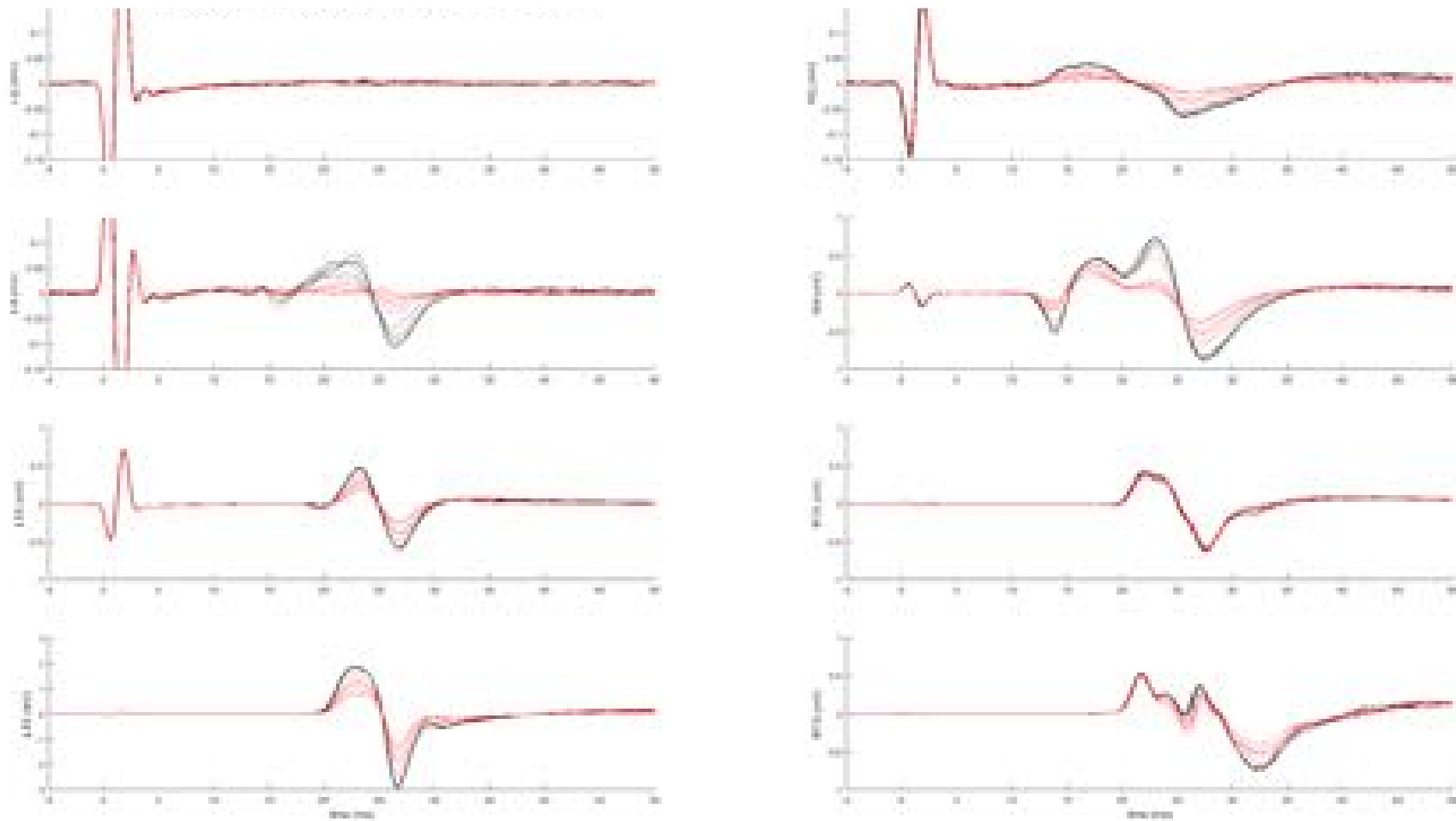
Electrical stimulation of peripheral nerves or posterior roots can activate monosynaptic and polysynaptic reflex arcs

Augmentation of residual neural control by non-invasive spinal cord stimulation to modify spasticity in spinal cord injured people



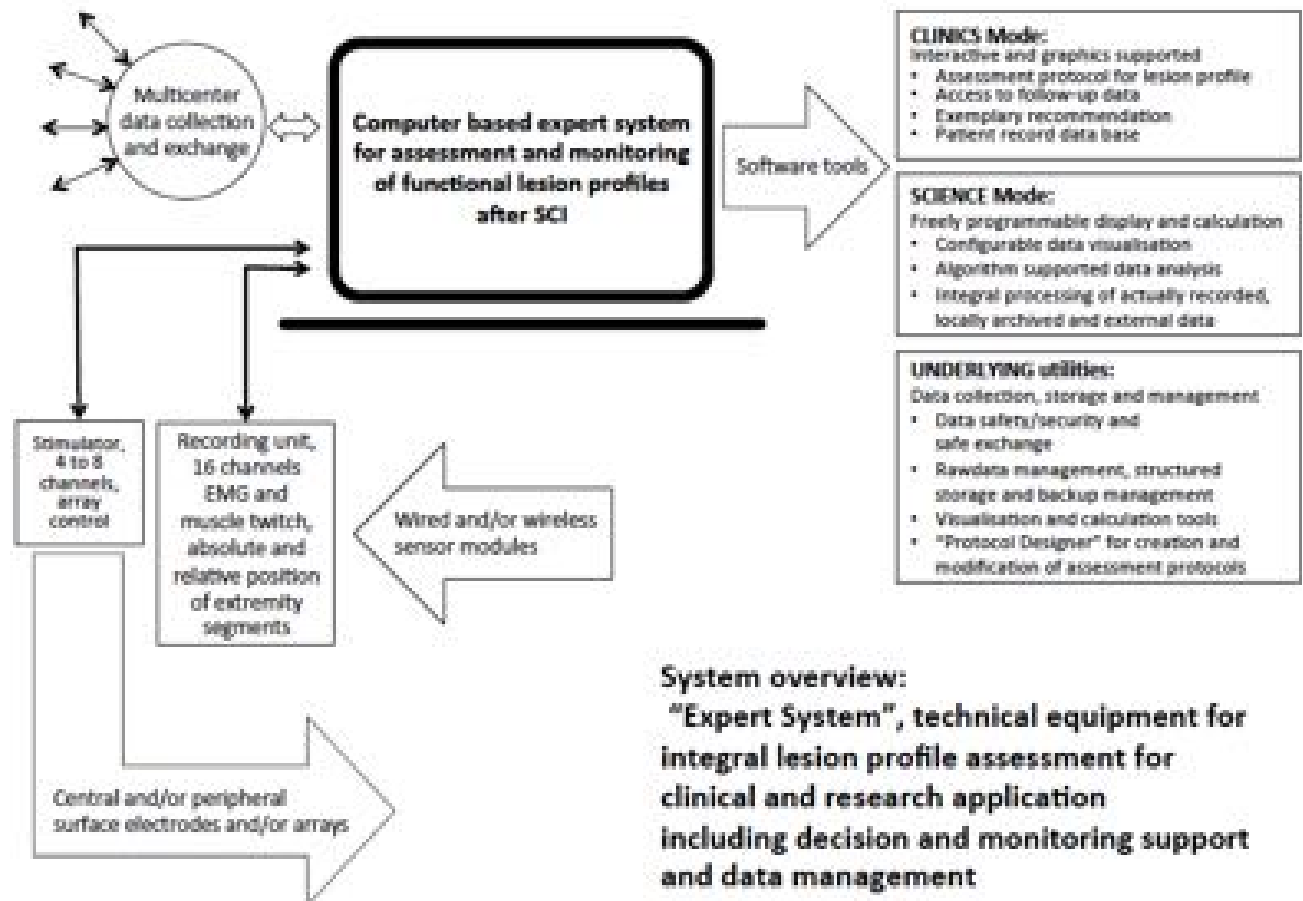
Posterior root reflex as marker for discompleteness

Modification of posterior root reflexes: Attempt to extend both legs (red), control (black)



Augmentation of residual neural control by non-invasive spinal cord stimulation to modify spasticity in spinal cord injured people

- BMCA
 - Reinforcement Maneuvers
 - Volitional Maneuvers
 - Passive Maneuvers
 - Reflex Modulation
- Bipolar Non-Invasive SCS
 - Recruitment curve
 - Frequency sweeps
- Personalization
(individual profile, altered and residual functions)
- Specific
planning and monitoring



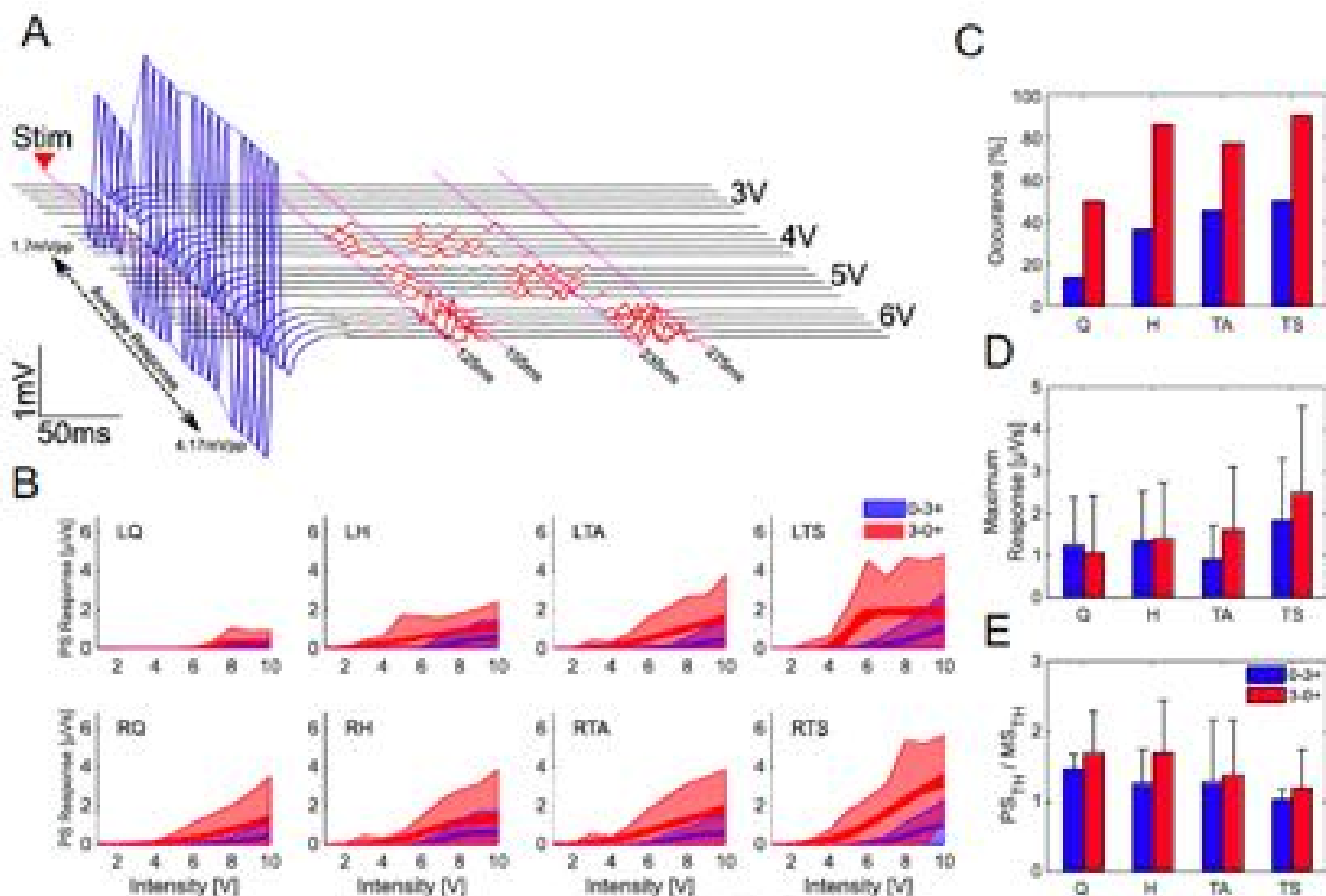
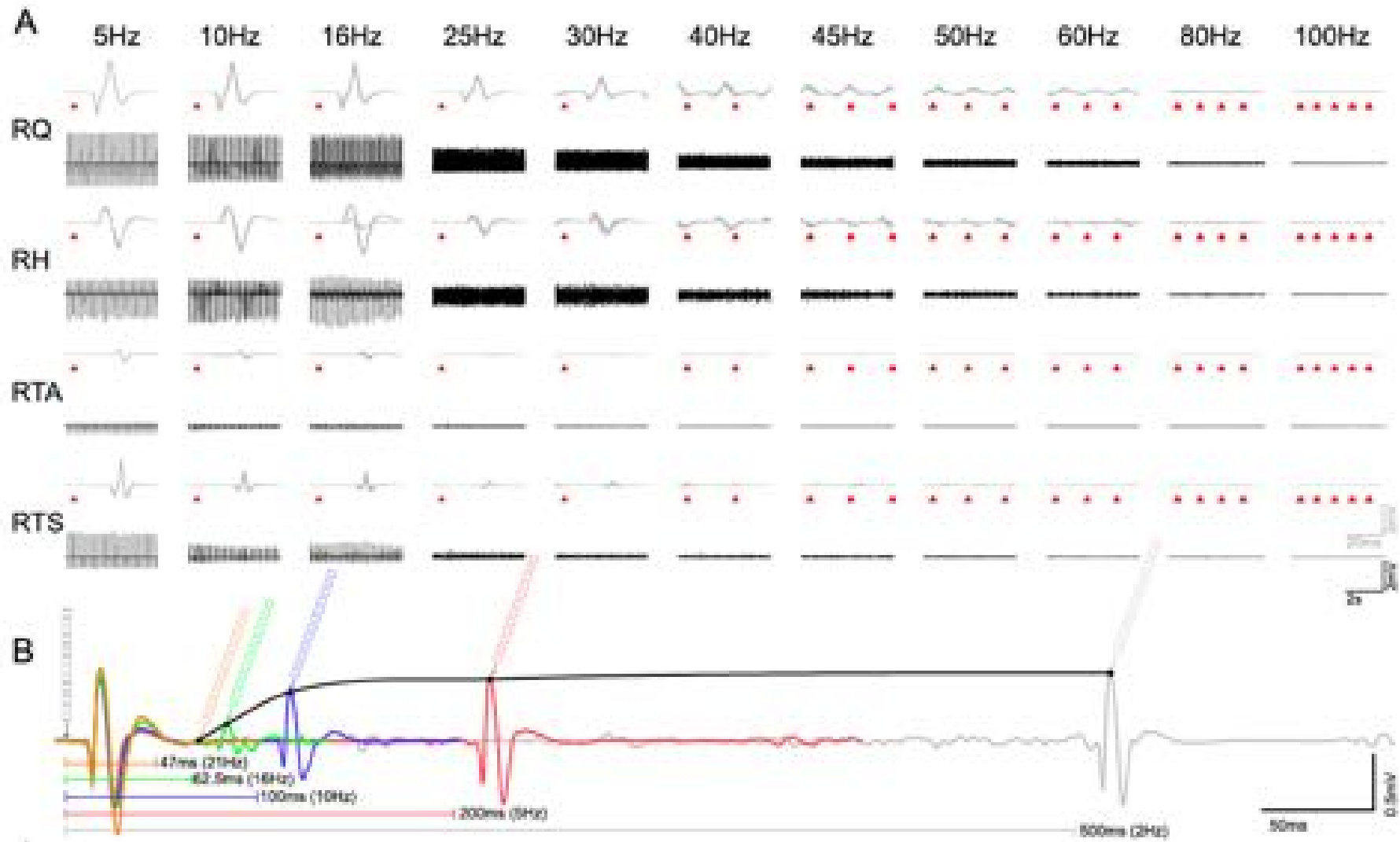


Fig. 2 Characteristics of the Polysynaptic responses. **A** Exemplary responses from RH on SID 10 with 3-0+ electrode configuration. The sEMG show in blue the short-latency (monosynaptic) responses, appearing after ~ 7 ms, and, in red, the long-latency (polysynaptic) responses, which appear in two groups with latencies of around 130 ms and 260 ms. Both types of responses evolve when the stimulus intensity is increased. **B** Estimated recruitment curve for eight subjects (SID2 and SID8 excluded), showing the 95% confidence interval for the mean amplitude (narrowband) and standard deviation

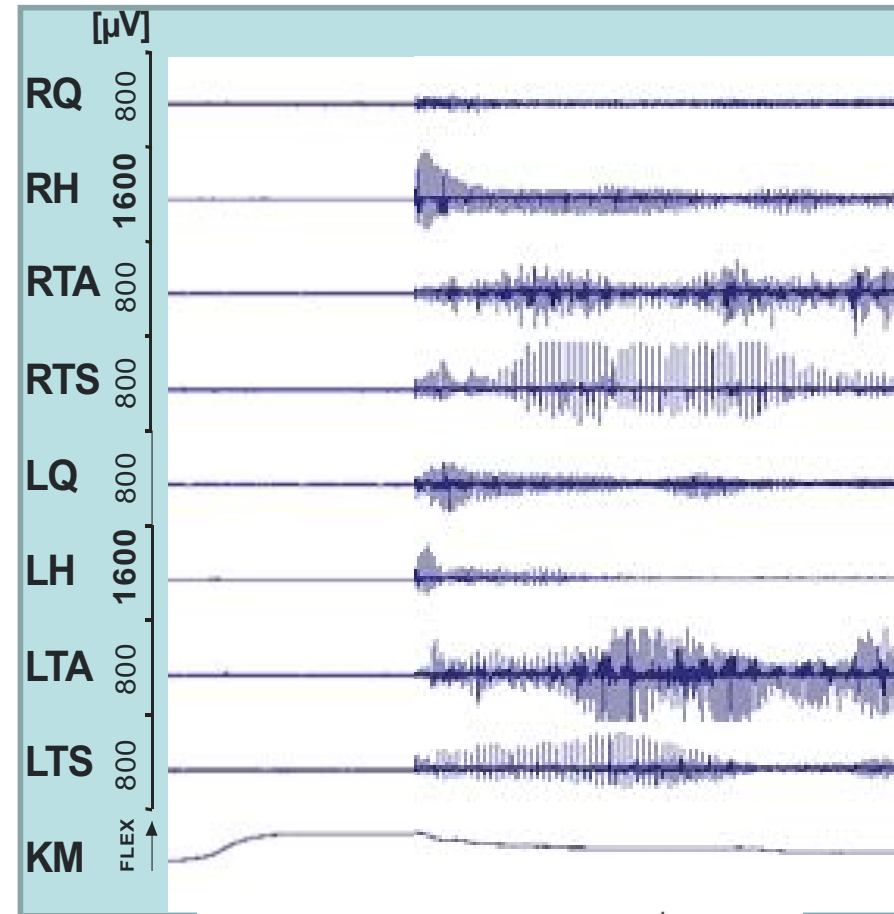
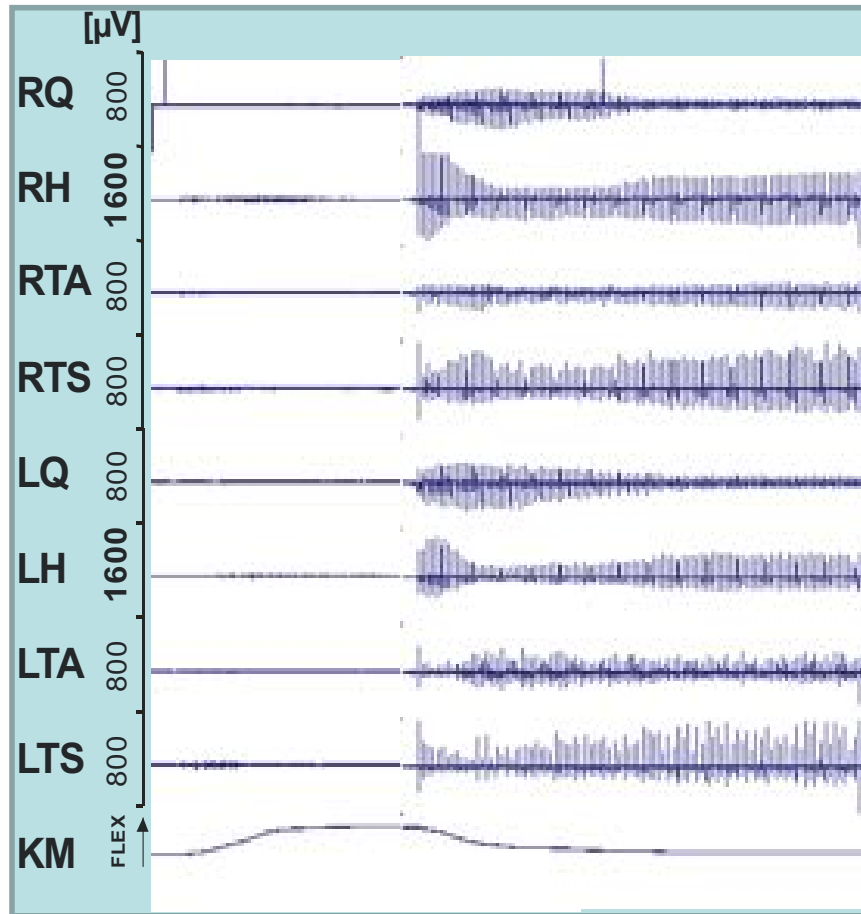
of the samples at each intensity (shadowed area) for the lower limbs with both electrode configurations. **C** Shows the percentage of polysynaptic activity occurrence on each muscle group (both sides grouped together). **D** shows the mean maximum response for each muscle and electrode configuration (SID8 excluded due to continuous activity not associated with the stimulation). Finally, **E** Shows the relative threshold of the polysynaptic activity compared to the monosynaptic activity



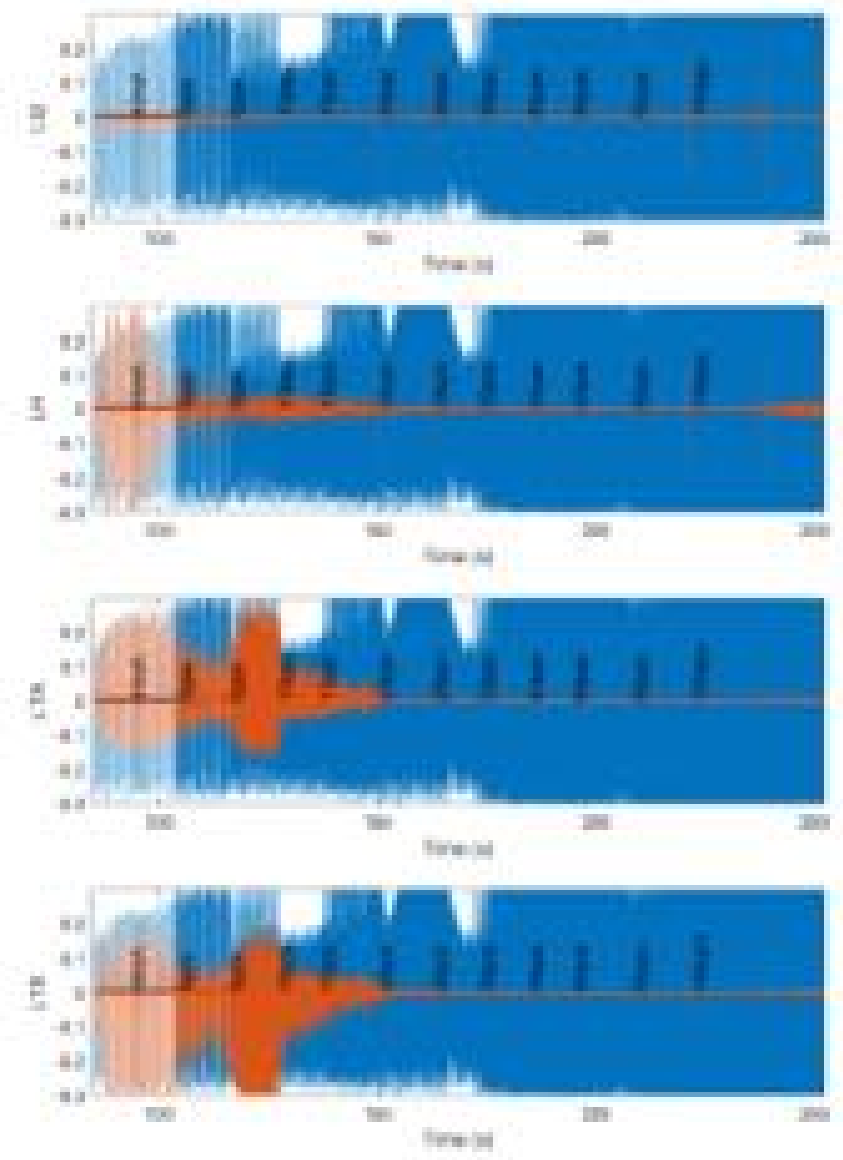
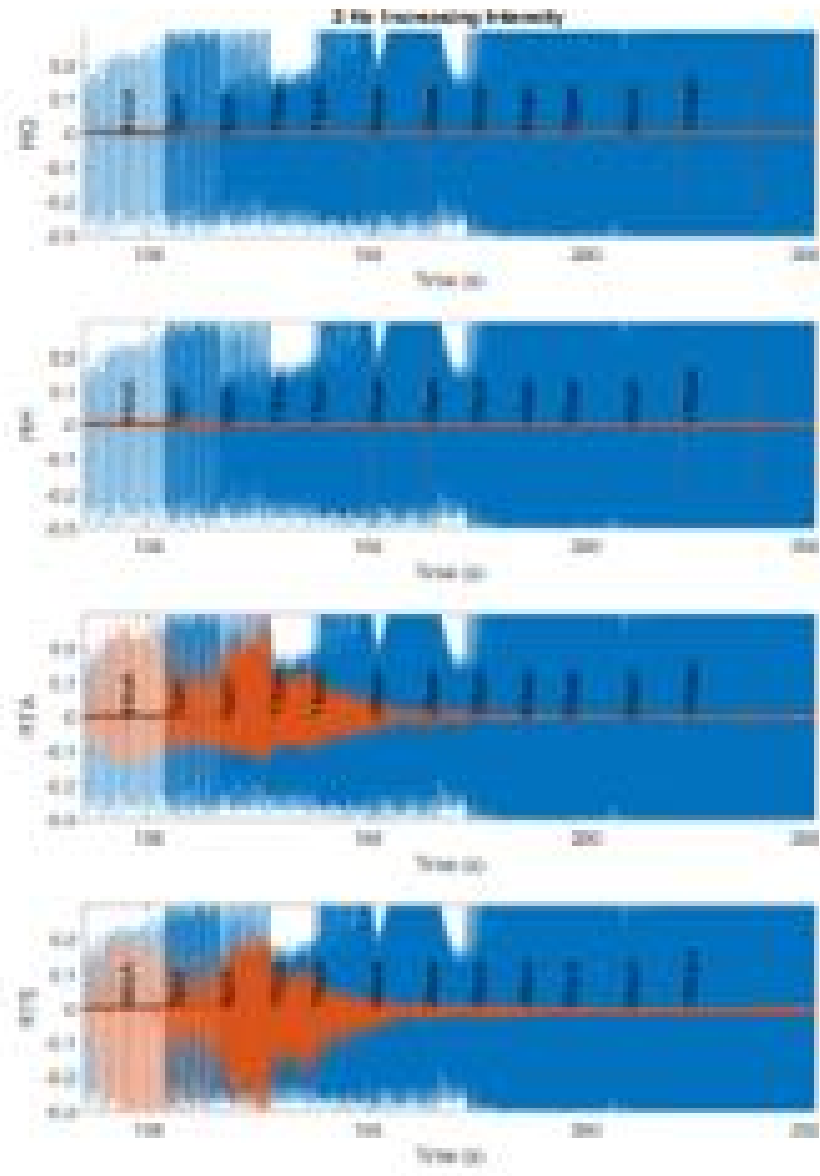
Effect of altered frequency on passively induced flexion

10V , 10Hz

10V , 16Hz



Frequency Sweep at 40mA
(Blue: Stimulation, Orange: EMG)



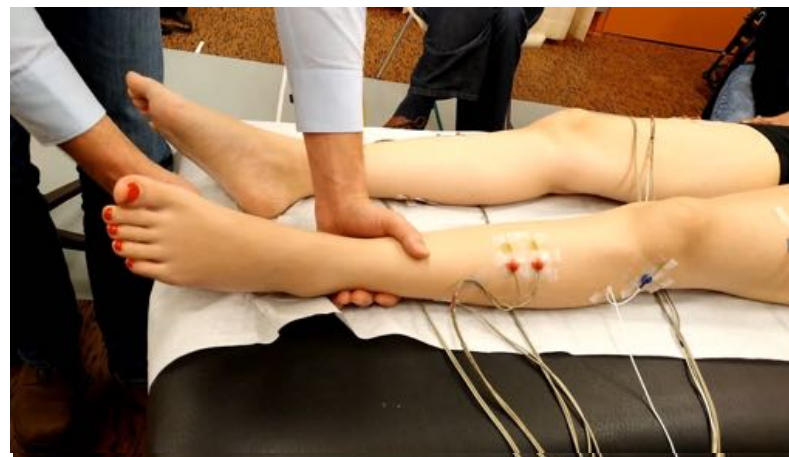
Augmentation of residual neural control by non-invasive spinal cord stimulation to modify spasticity in spinal cord injured people

Main results and impact

Babinski

NO stimulation

10pps / 20mA

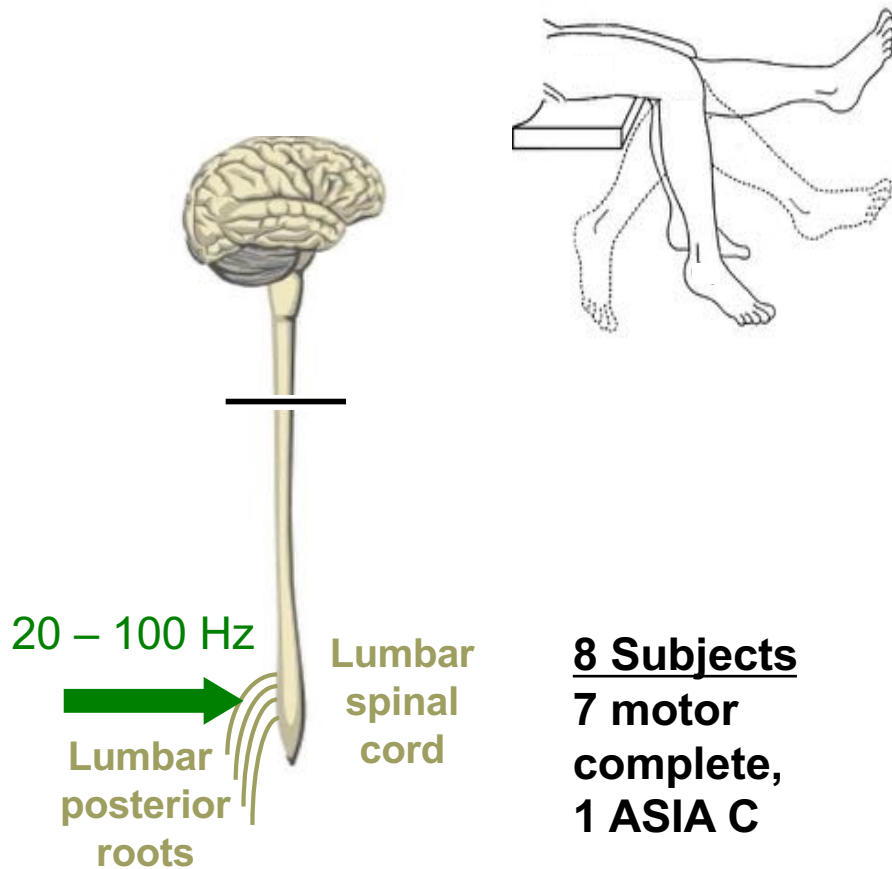


50pps / 40mA



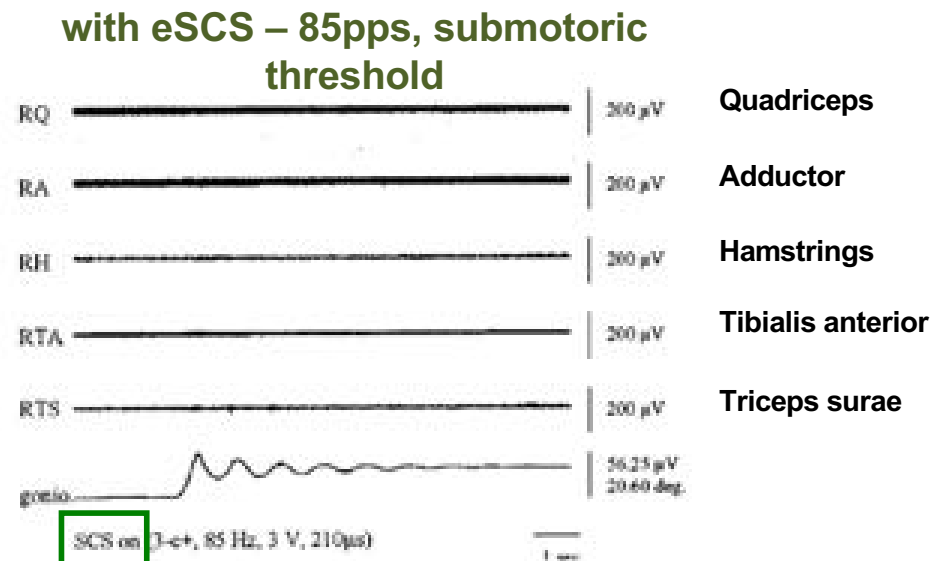
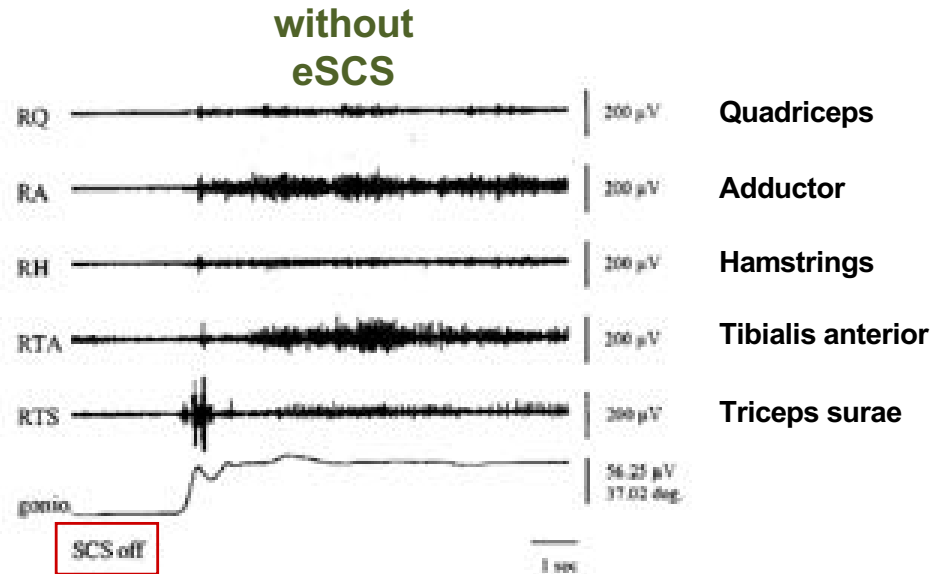
Control of spasticity

Assessment of spasticity using the Pendulum test

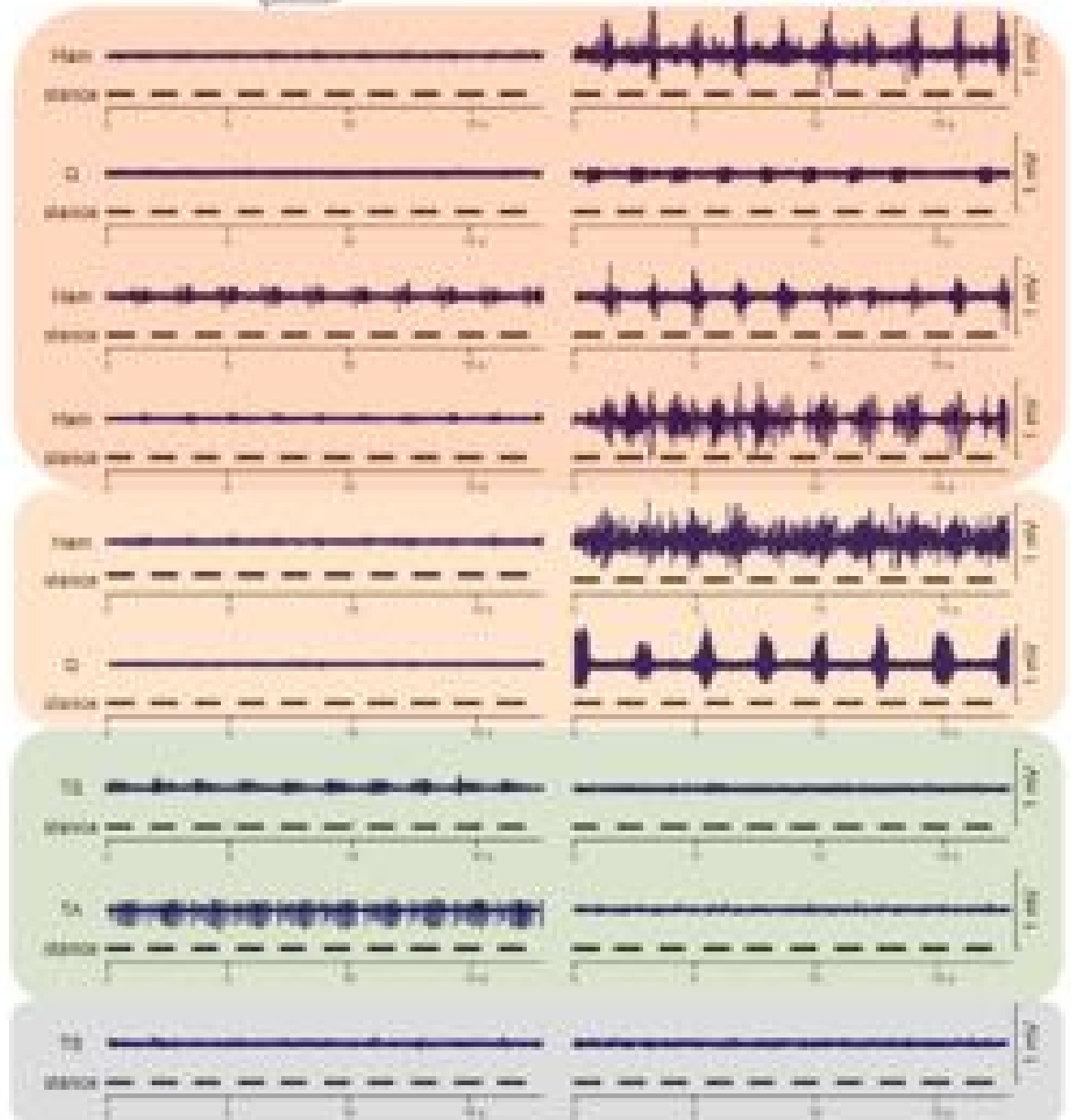
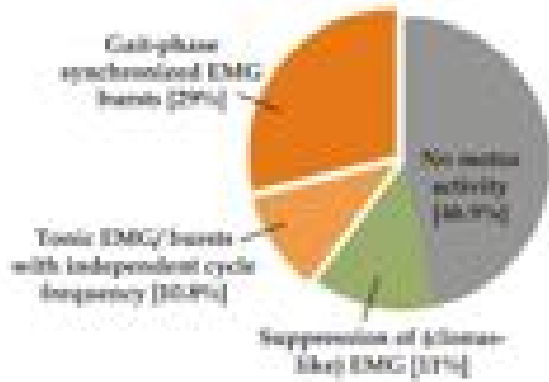


8 Subjects
7 motor complete,
1 ASIA C

Traumatic SCI
C5 to T6

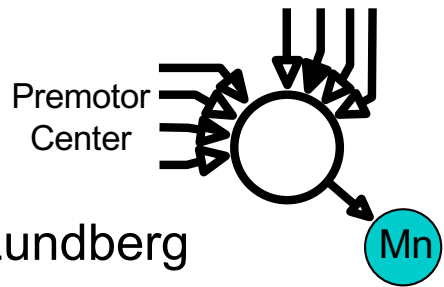


effect groups:

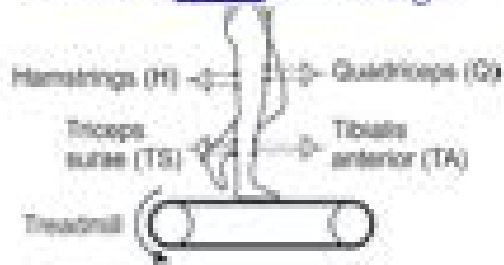


1979

Anders Lundberg



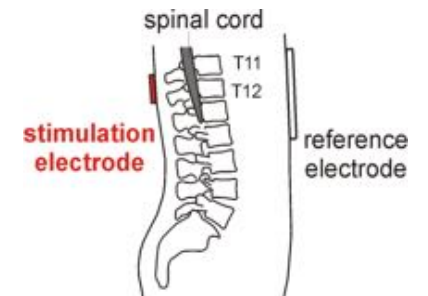
Surface EMG recordings:



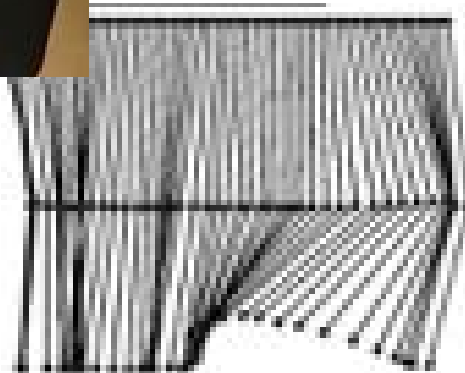
Facilitation of stepping in incomplete SCI by tSCS



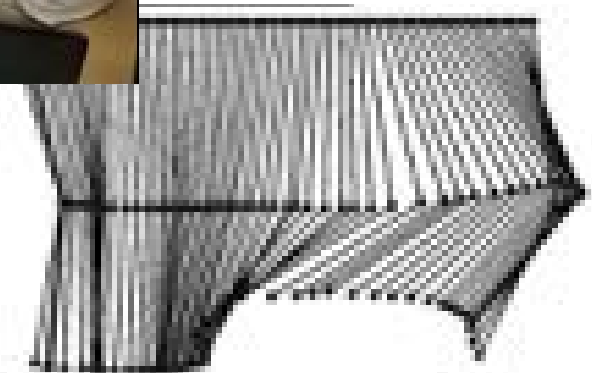
Subject:
ASIA D, T8-T9



1.6 km/h; no stimulation



1.6 km/h
tSCS: 30 Hz, 18 V



Facilitation of functional standing and walking in wheel-chair bound spinal cord injured people by spinal cord stimulation: Study of neurocontrol and biomechanical output
WFL-FR-001/06

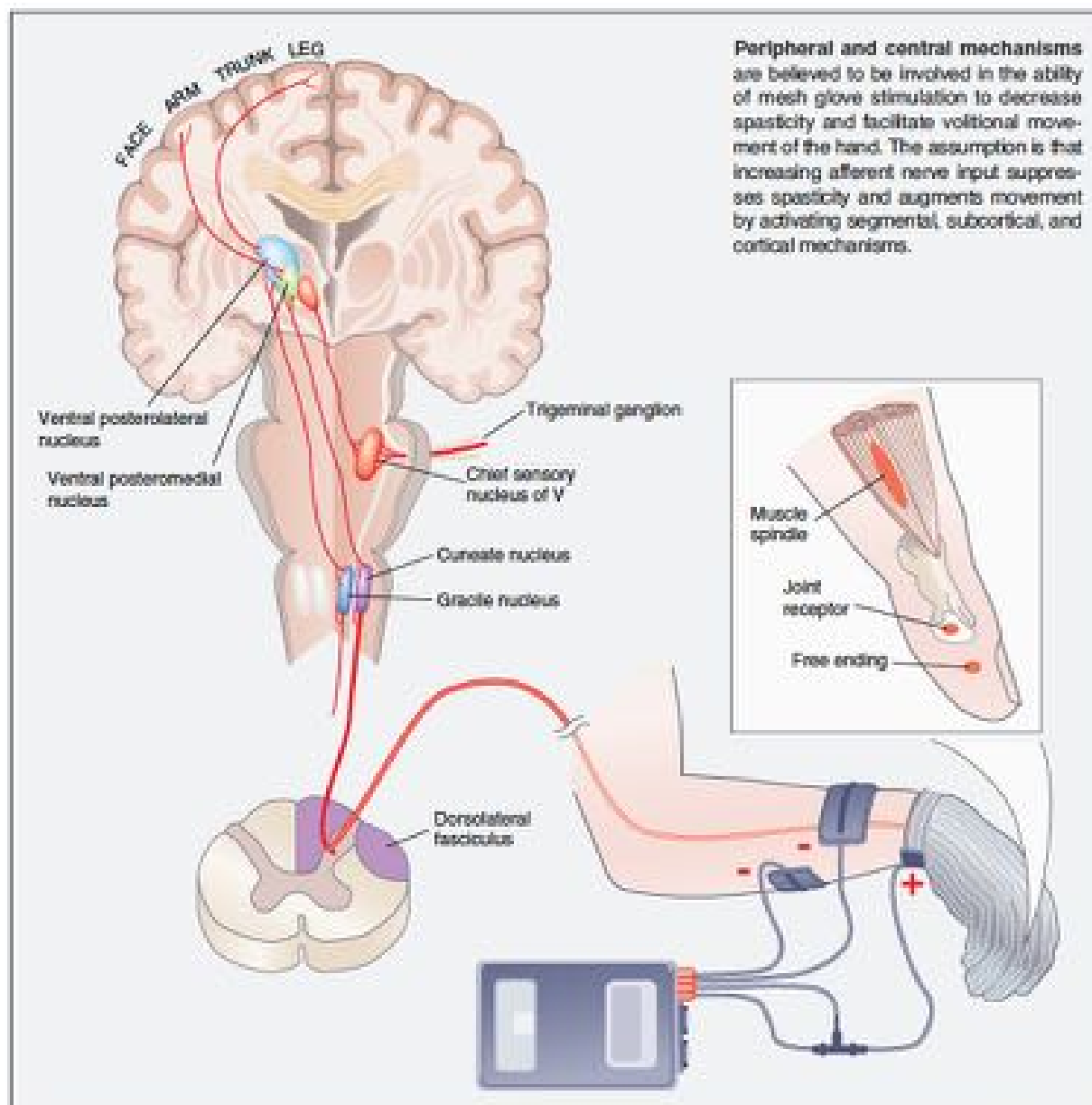
Dimitrijevic MR
Clinical practice of FES: From “Yesterday” to “Today”
Artificial Organs. 2008 Aug;32(8):577-80

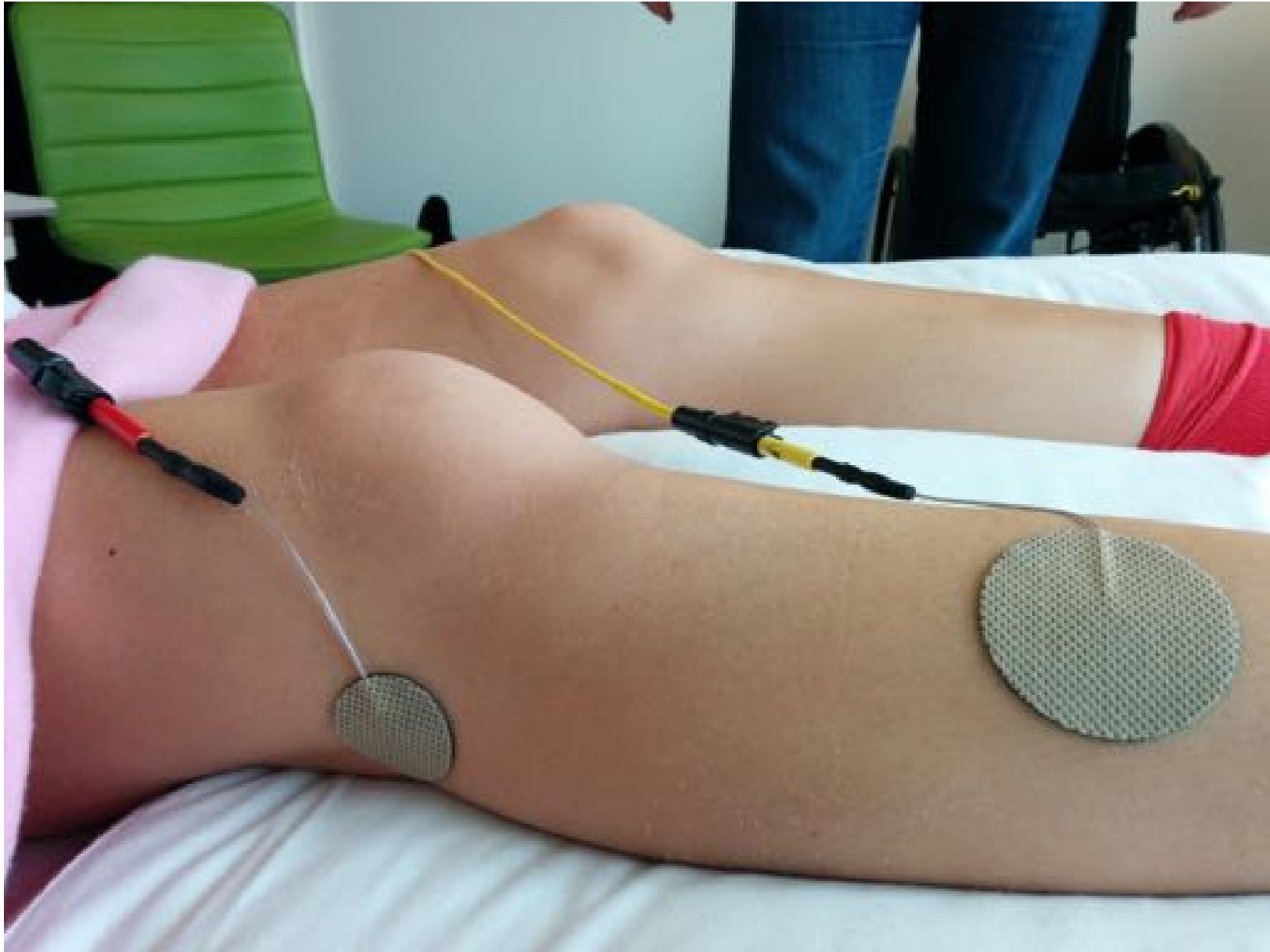
Mesh Glove Electrical Stimulation

by M. Meta Dimitrijević, Nachum Soroker,
and Fabian E. Pollo

SCIENCE & MEDICINE

May/June 1996





Peroneal Nerve

subsensory continuous: 1a afferents

-

supra-motor-threshold: withdrawal

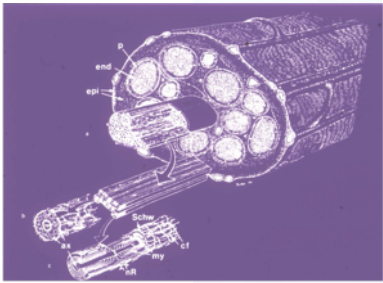


EXOPULSE Mollii Suit
Stockholm, Sweden

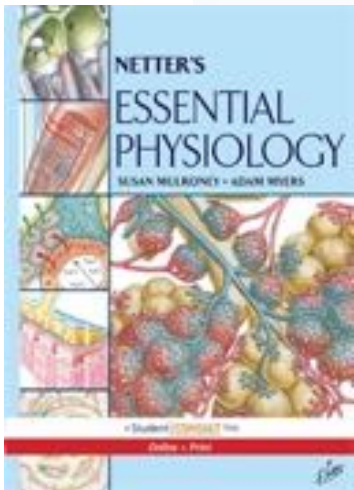
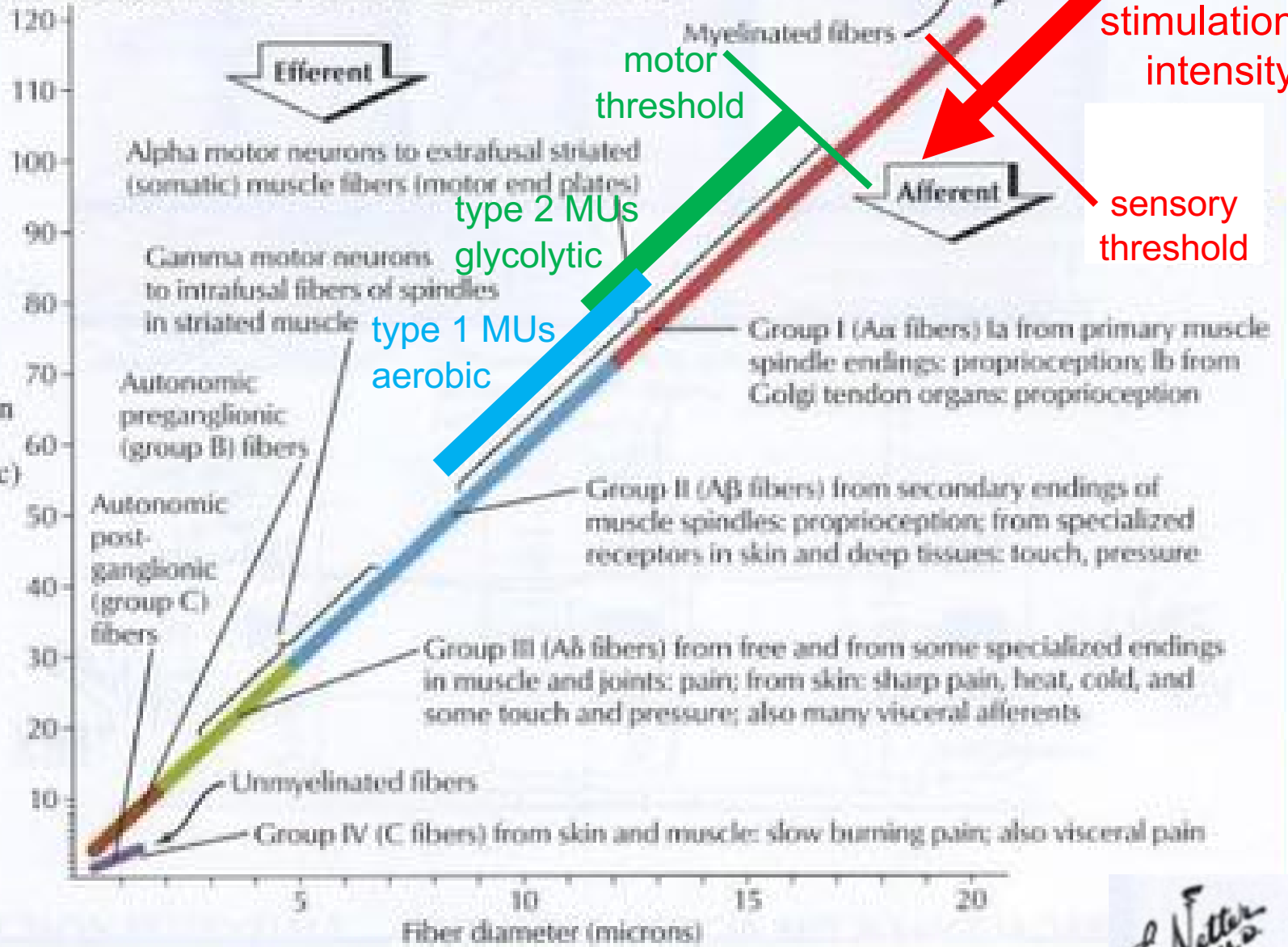
 EXOPULSE

ottobock.

C. Classification of nerve fibers by size and conduction velocity

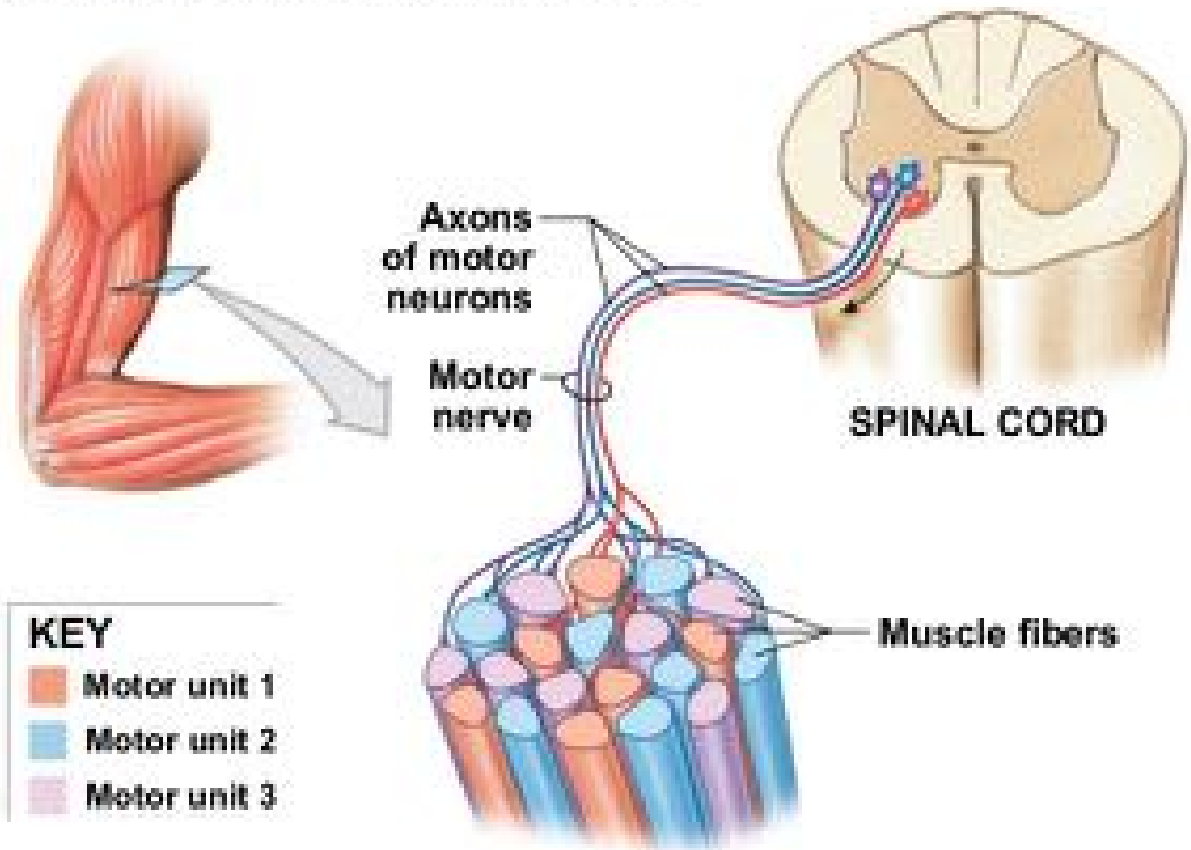


Conduction velocity (meters/sec)



SELECTIVITY

Figure 9.12 The Arrangement of Motor Units in a Skeletal Muscle



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MIXED NERVE, predominantly afferent
 Glycolytic & aerobic motor units –
 - mixed morphology in nerve and muscle
 Control-, metabolic and biomechanical issues

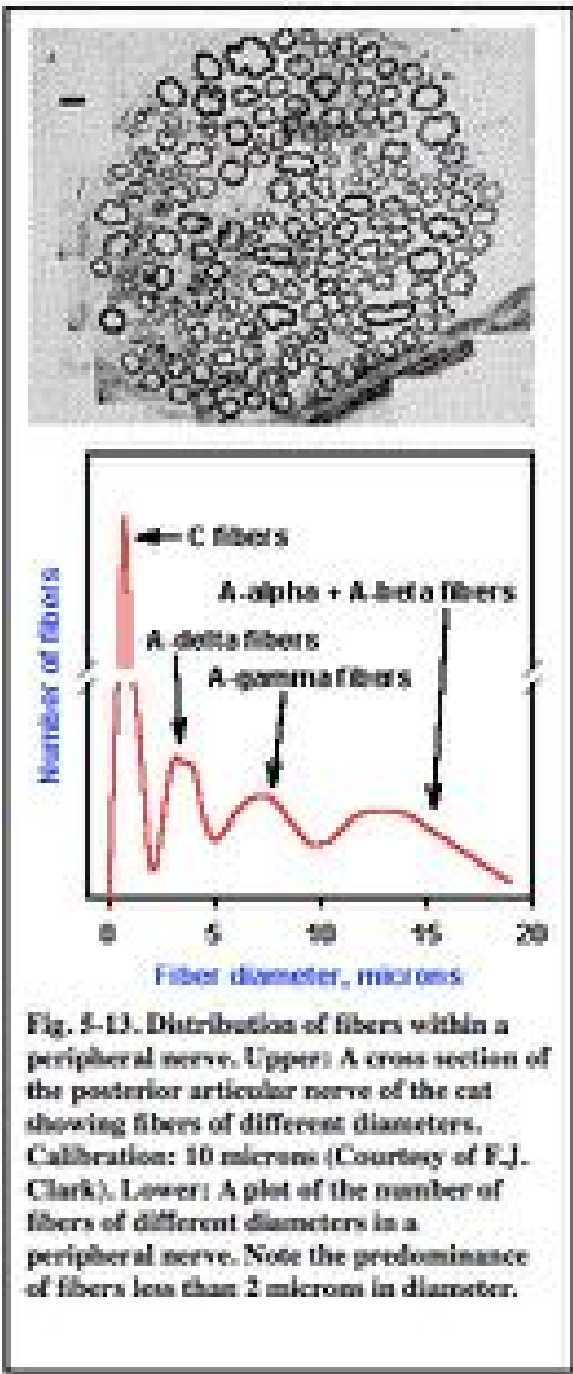
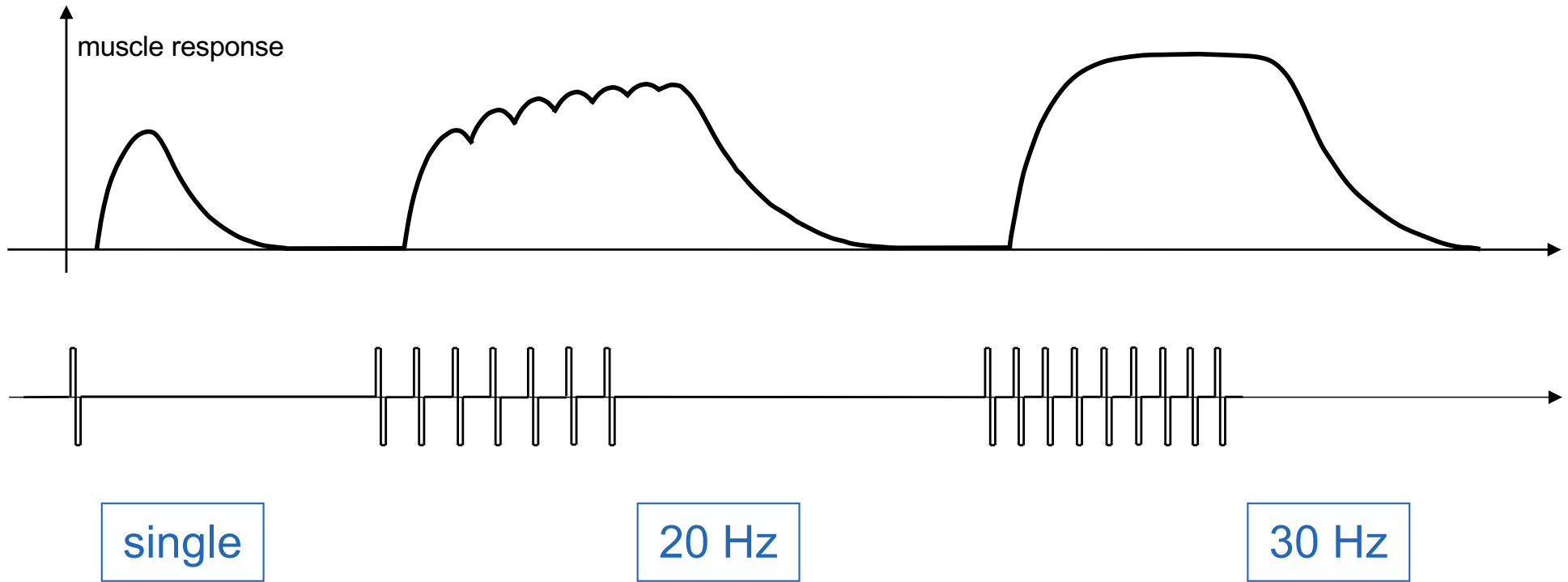
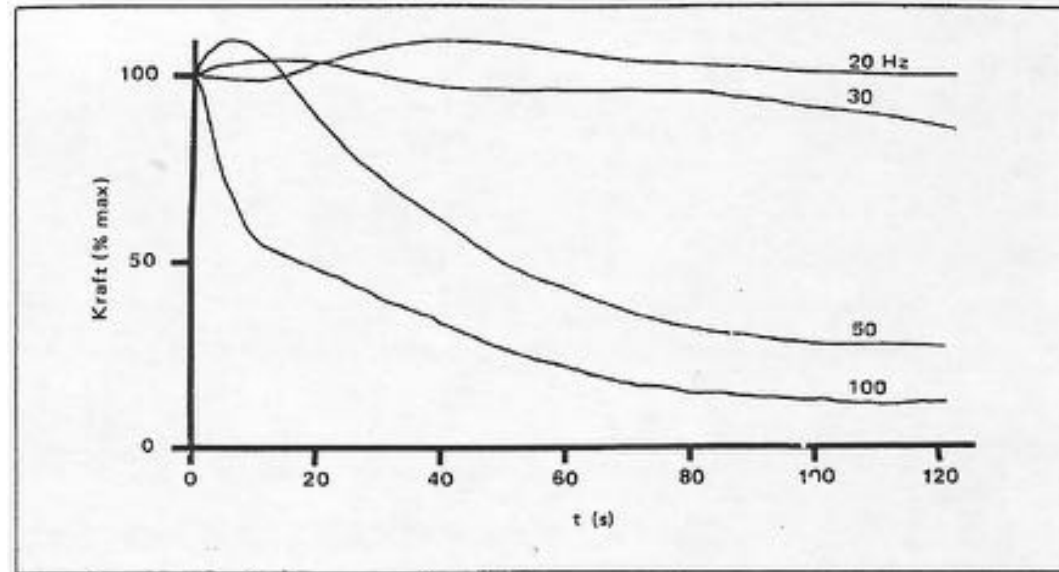
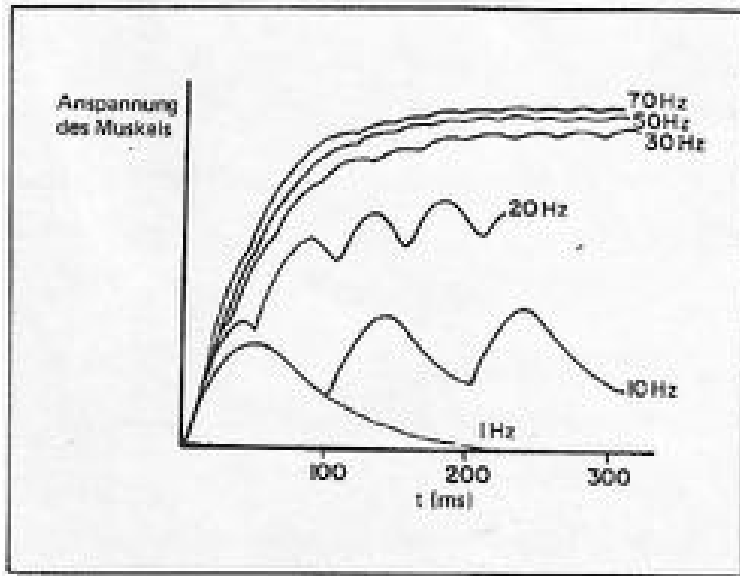


Fig. 9-13. Distribution of fibers within a peripheral nerve. Upper: A cross section of the posterior articular nerve of the cat showing fibers of different diameters. Calibration: 10 micrometers (Courtesy of F.J. Clark). Lower: A plot of the number of fibers of different diameters in a peripheral nerve. Note the predominance of fibers less than 2 micrometers in diameter.

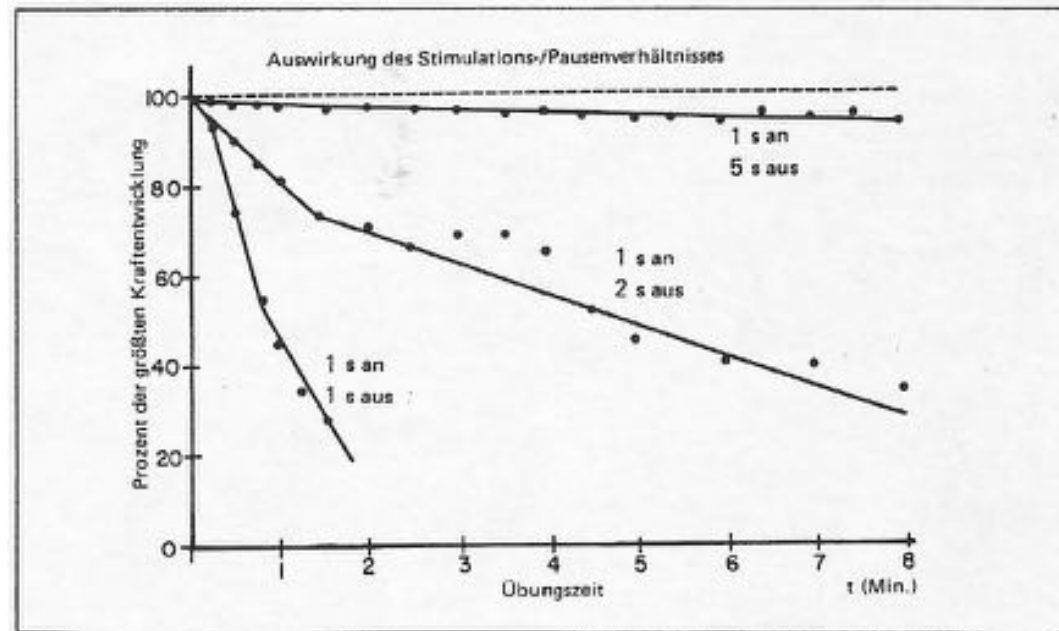
Michael D. Mann:
 The Nervous System in Action
<http://michaeldmann.net>



Frequency dependence of contraction force development and muscle fatigue

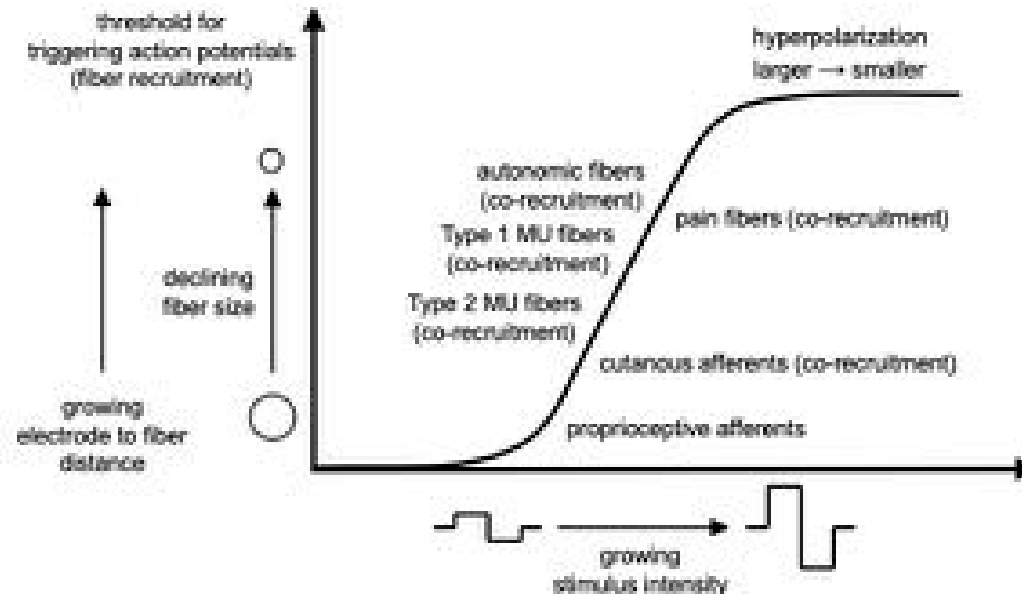


ON-/OFF-relation dependence of muscle fatigue



Summary

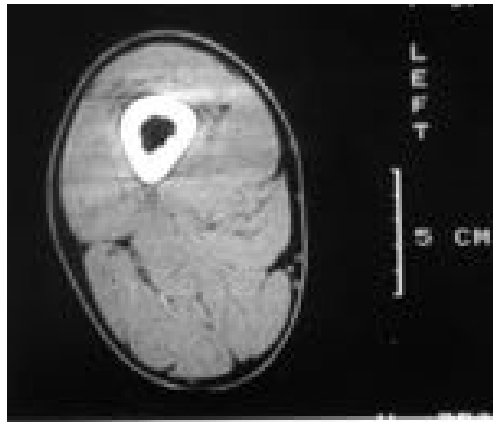
Stimulation interface – neuron activation



- Size and distance dependent **recruitment** of fibers (in groups)
 - Lowest threshold – large afferents
 - Growing intensity co-recruits smaller fibers gradually
- Synchronous start – dispersion by distance and conduction velocity
- Beyond recruitment - **frequency** influences
 - central interneuron **processing** as **afferent** input
 - **contraction** properties in **efferent** neuromuscular activation

Consequences of muscle denervation

Healthy thigh

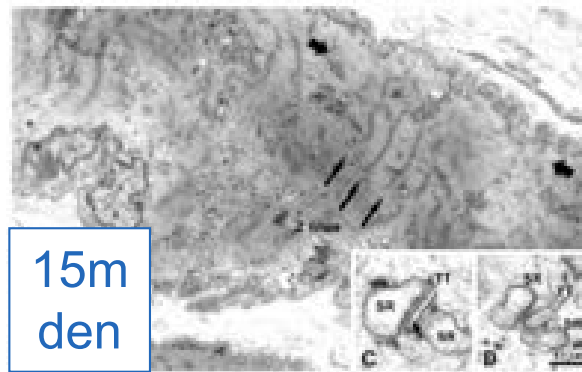
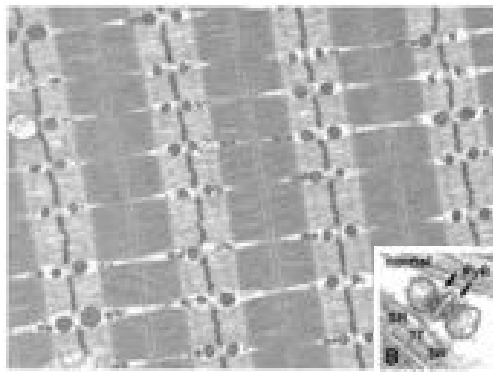
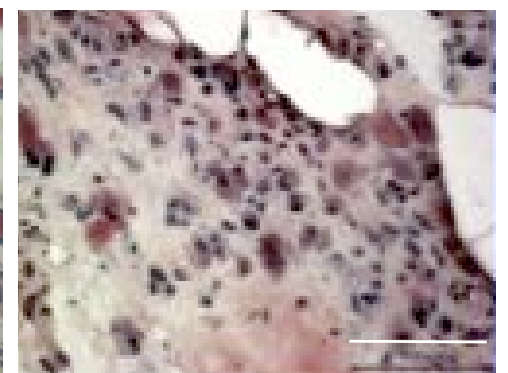
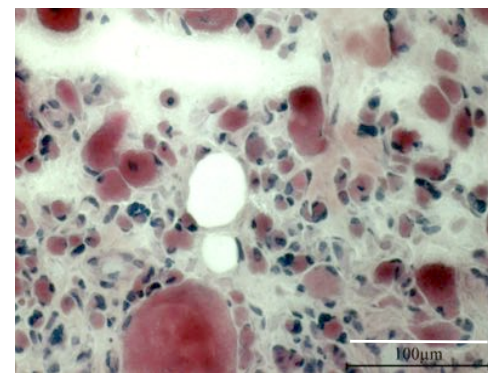
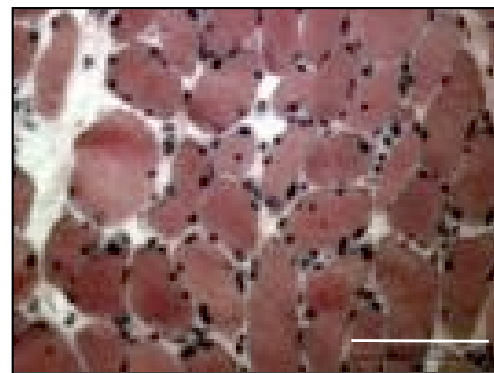
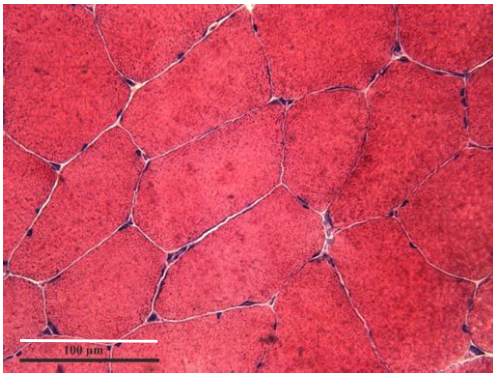


0,9y
den

4 years denervated



8,7 years denerv.



15m
den

MFCV _{max} vastus lat:	
healthy	4,48 m/s
10mo den	2,40 m/s
30mo den	1,20 m/s

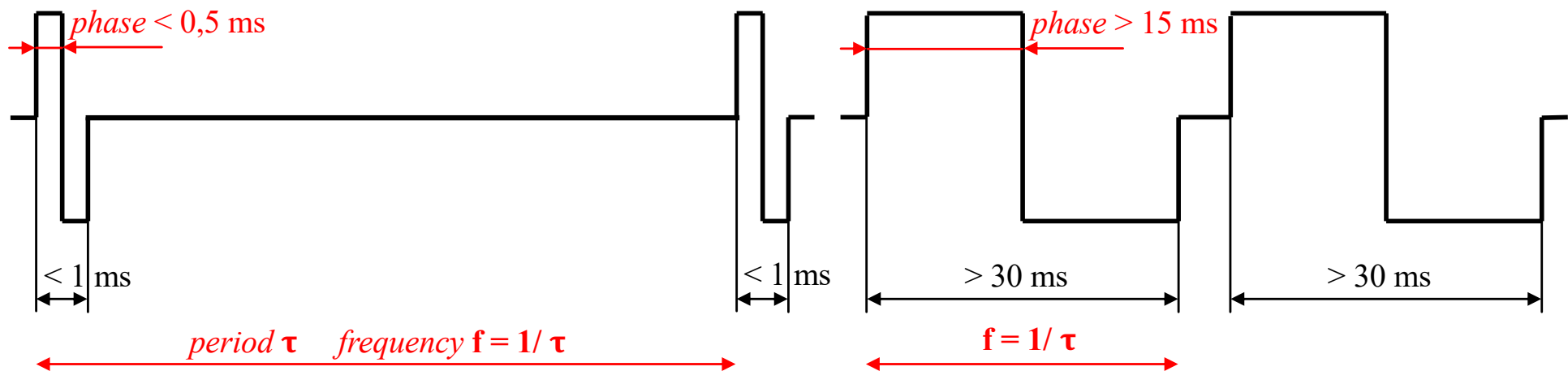
Stimulation parameter ranges

Nerve stimulation:

- Pulse width (biphasic)
typ. $< 0.5\text{ms}$ per phase
- Frequency (fused contr.)
25 Hz
- Amplitude range (Surface)
 $\Rightarrow \pm 100\text{V} / \Rightarrow \pm 300\text{mA}$
- Amplitude range (Implant)
 $\Rightarrow \pm 10\text{V} / \Rightarrow \pm 30\text{mA}$

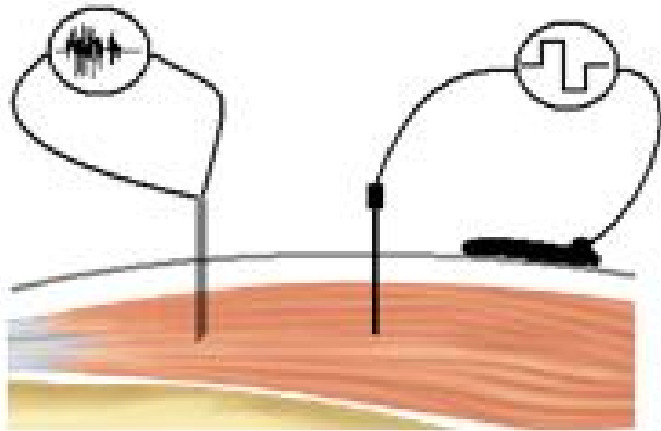
Muscle stimulation:

- Pulse width (biphasic)
typ. $> 15\text{ms}$ ($\Rightarrow 250\text{ms}$) per phase
- Frequency (fused contr.)
25 Hz
- Amplitude range (Surface)
 $\Rightarrow \pm 100\text{V} / \Rightarrow \pm 300\text{mA}$
- Amplitude range (Implant)
 $\Rightarrow \pm 10\text{V} / \Rightarrow \pm 30\text{mA}$

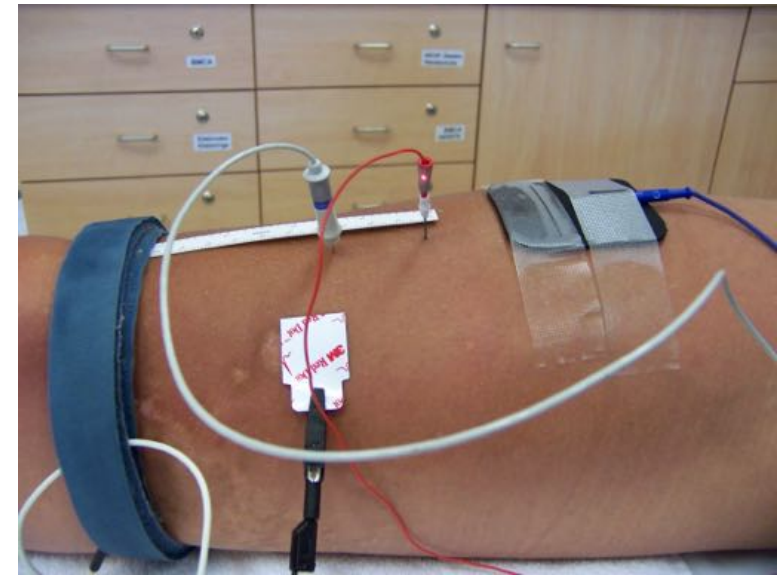
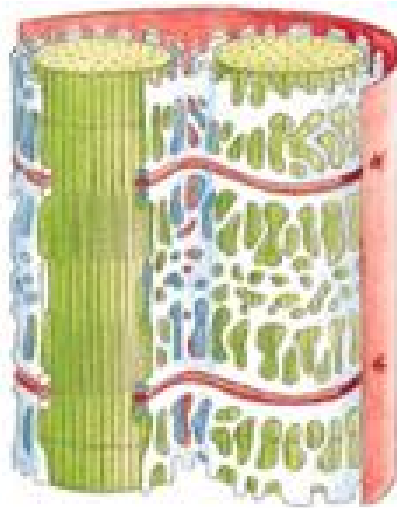


Single fiber recording

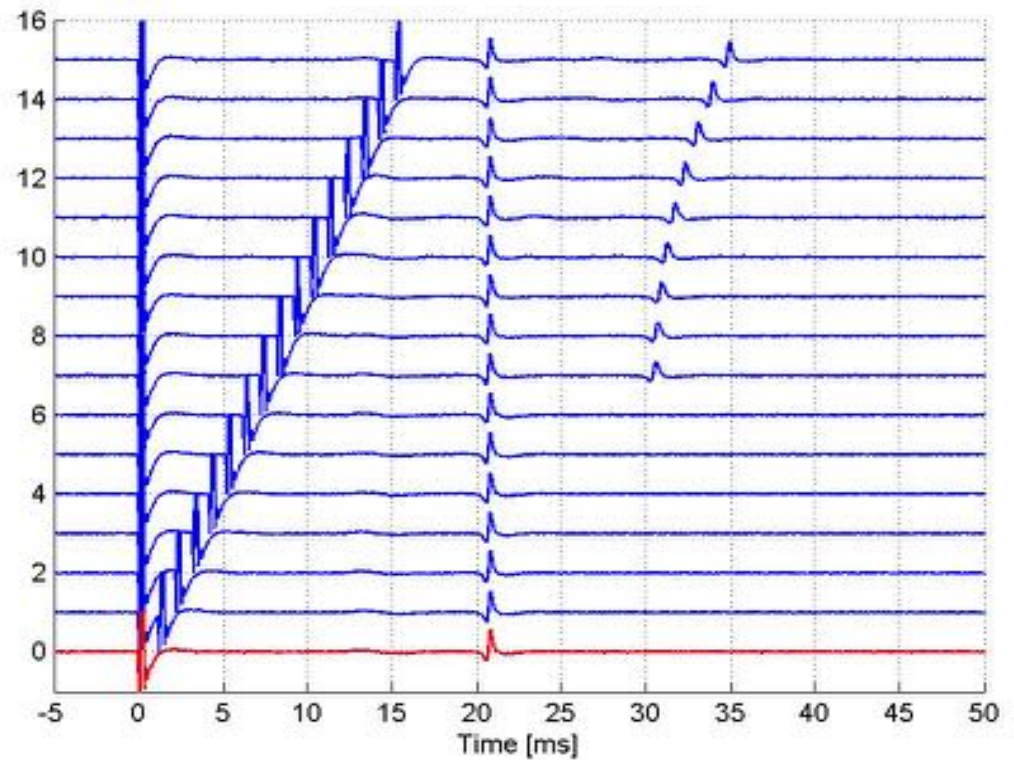
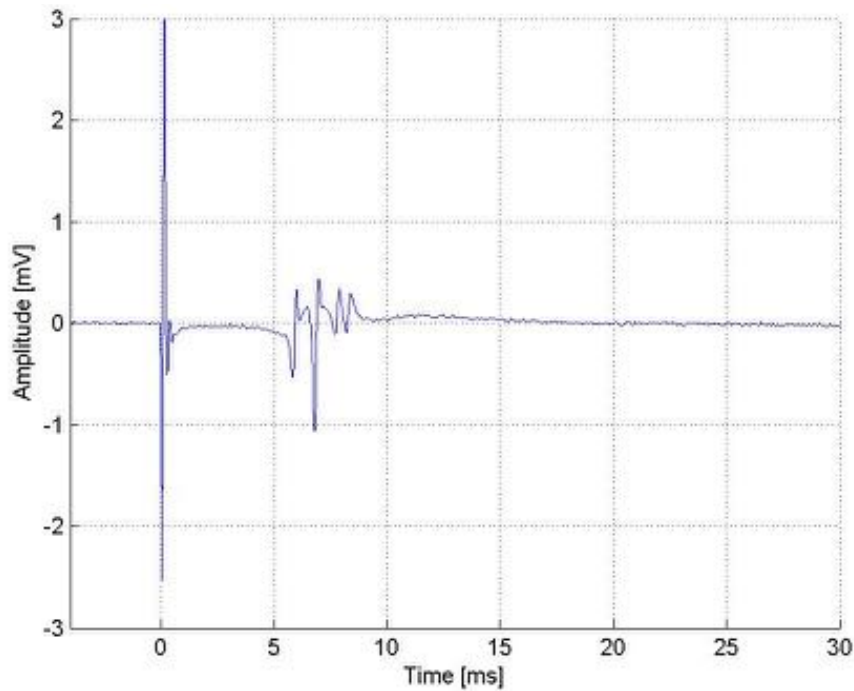
(PhD-Thesis Christian Hofer 2008)

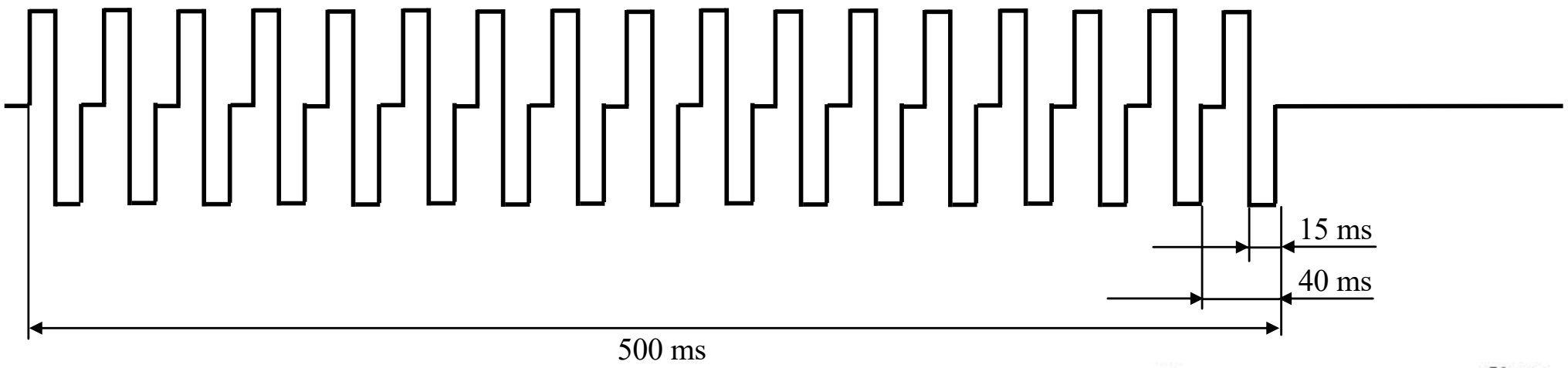
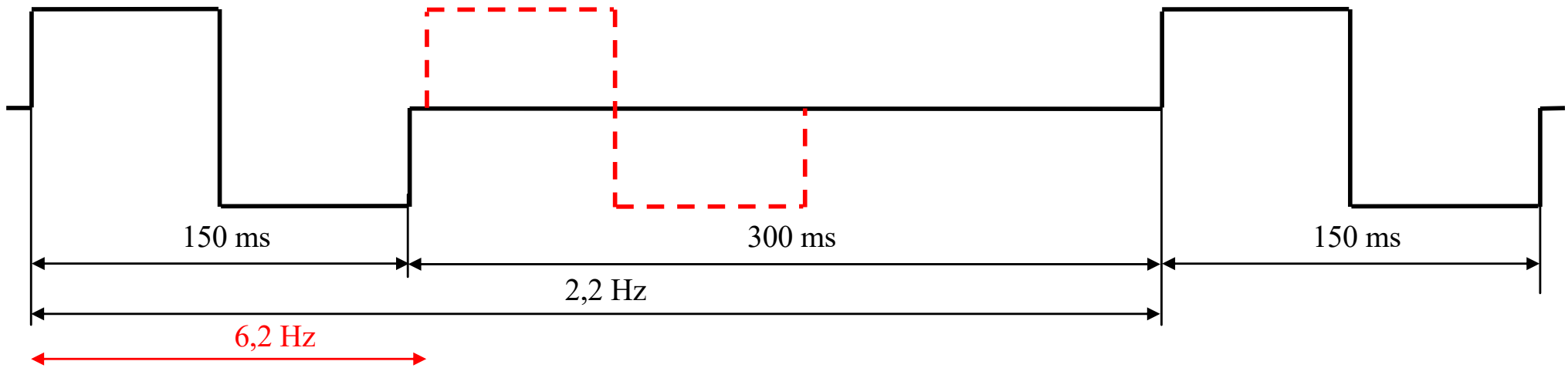


Single stimulus response



Double stimulus response

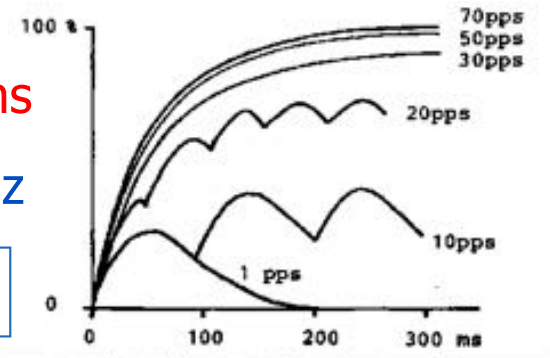




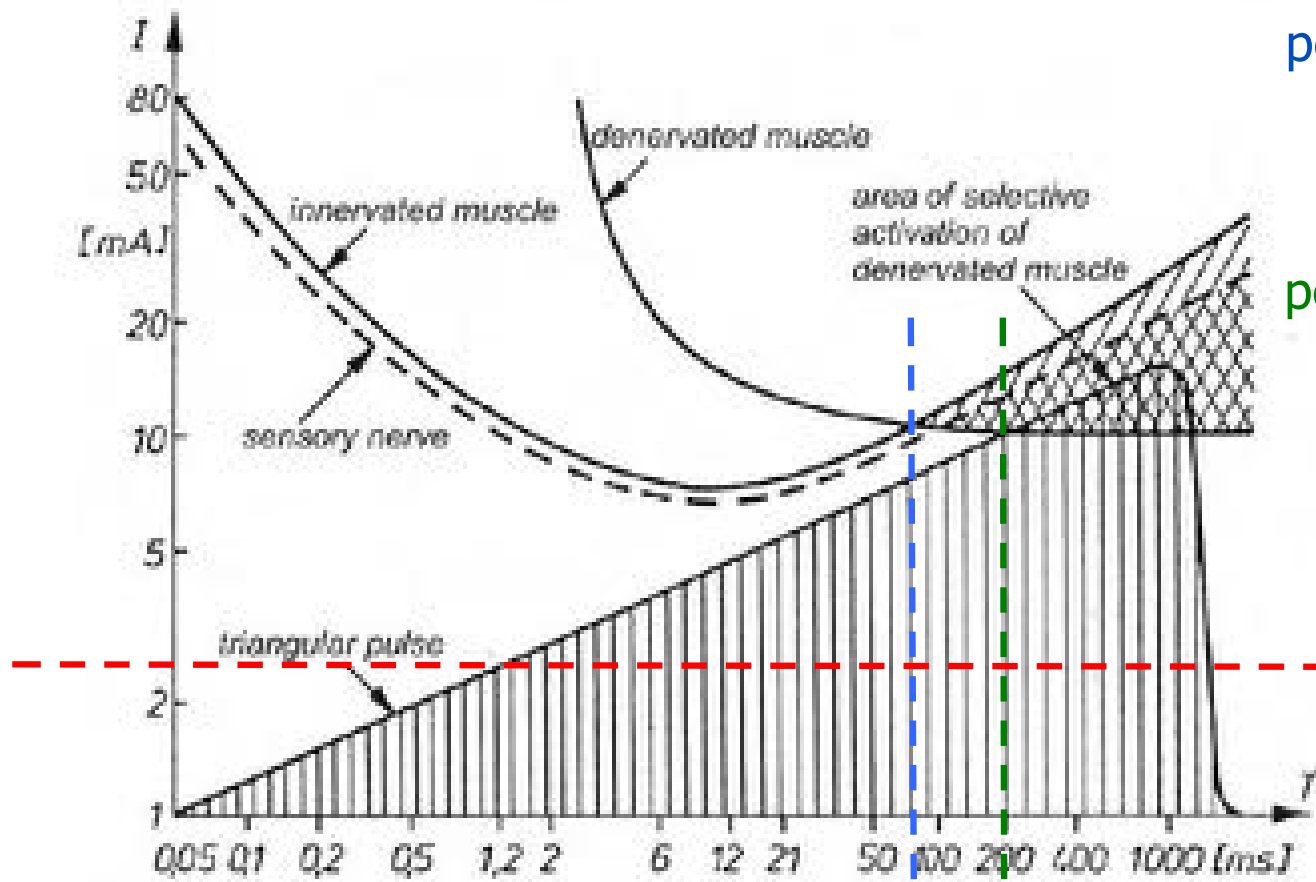
Excitability
conditioning

Period < 50 ms
> 20 Hz

Pulse phase > 15 ms
Period 40ms / 25 Hz



Single twitch ⇒ unfused tetanus ⇒ fused tetanus



periode = 80 ms

12,5 Hz

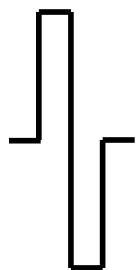
periode = 200 ms

5 Hz

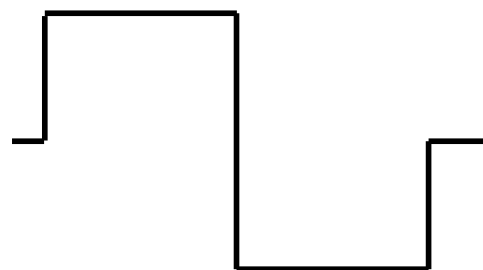
(10 / 15 mA)

DC

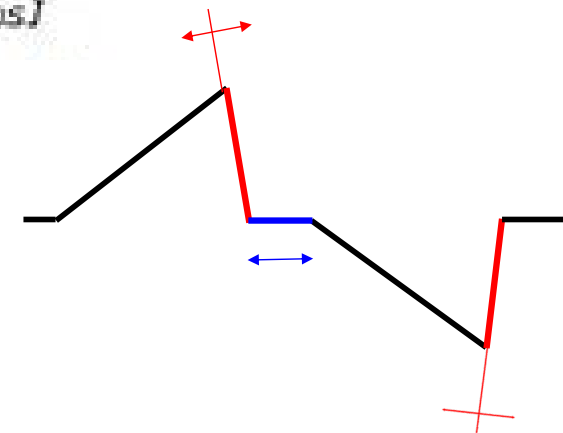
direct current component
in classical exponential current



nerve stimulation



muscle stimulation



muscle stimulation,
reduced nerve stimulation



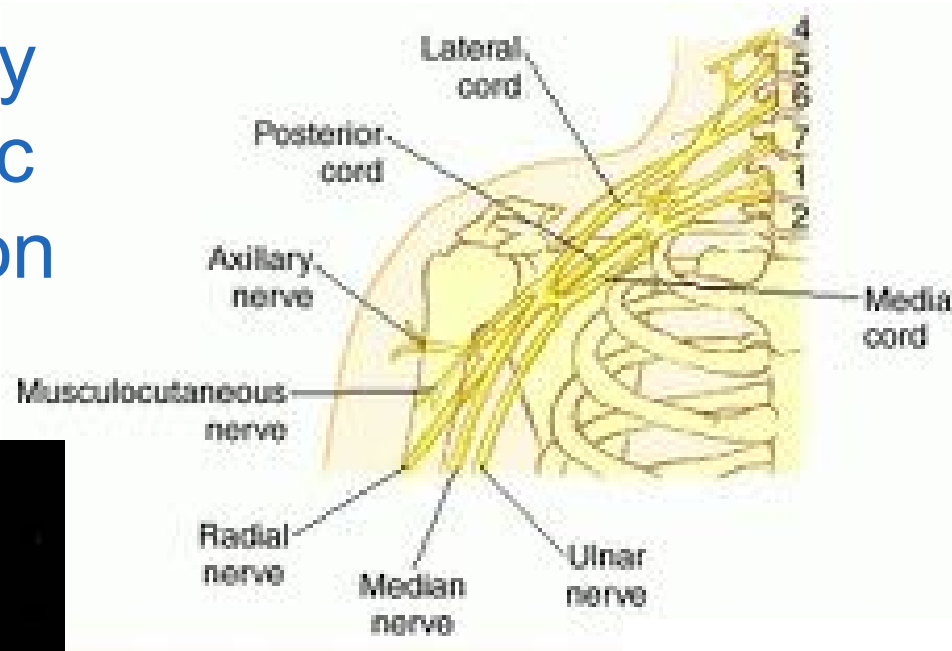
sub C5/C6, AIS A
5 years post injury
2x / week, 20min:
Single twitch FES, low
frequency, 80ms per
phase and pause

biphasic rectangular
30 Hz, 1ms/phase

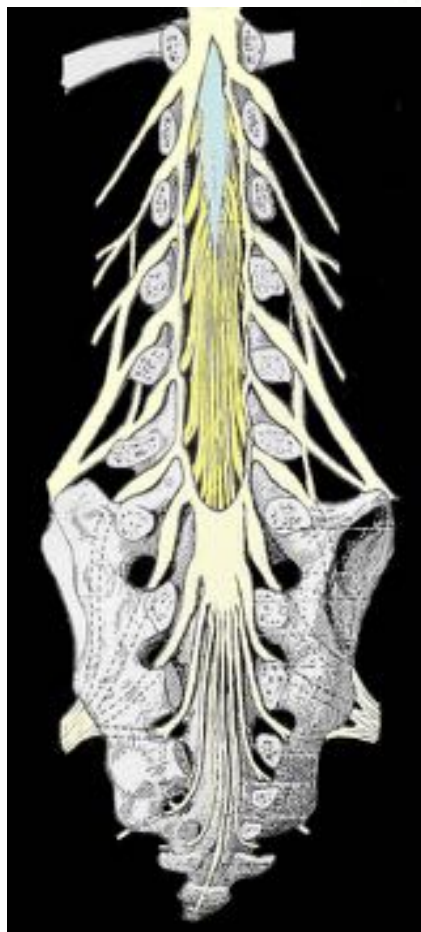
biphasic ramp
150ms/phase
150ms pause



Temporary or chronic denervation

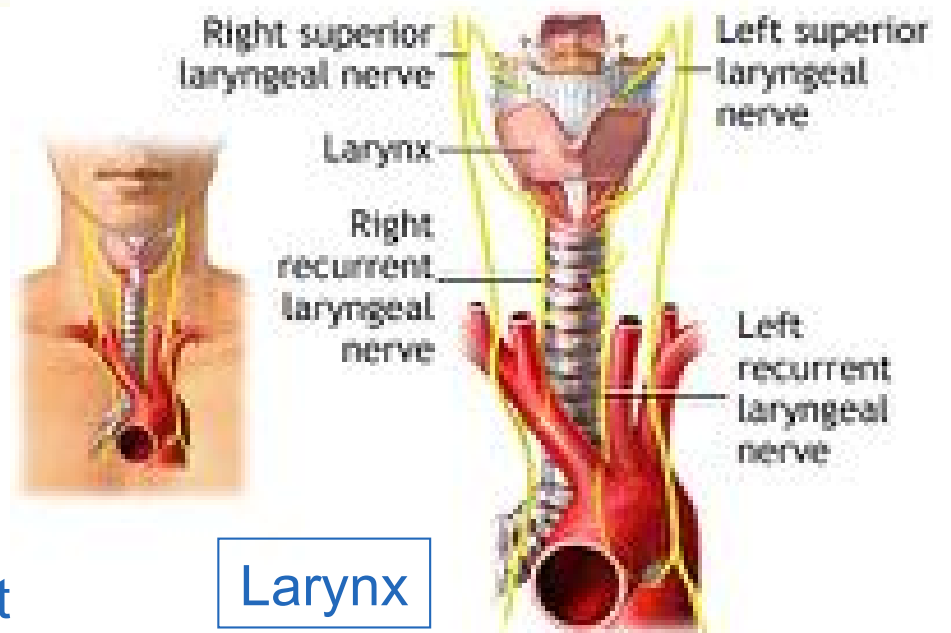


Facialis



Plexus

Cauda



Larynx

Recovery support
Reconstructive surgery



implant

ASIA IMPAIRMENT SCALE

A – Complete: No motor or sensory function preserved in the sacral segments S4-S5.

B – Incomplete: Sensory but not motor function preserved below neurological level and includes the sacral segments S4-S5.

C – Incomplete: Motor function preserved below neurological level, and more than half of key muscles below the neurological level have muscle grade below 3.

D – Incomplete: Motor function preserved below neurological level, and more than half of key muscles below the neurological level have muscle grade of 3 or more.

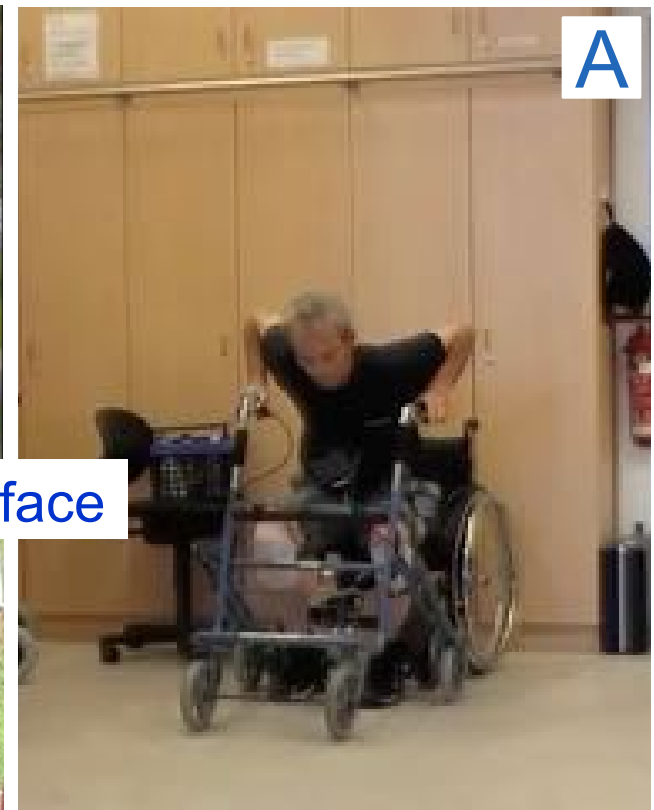
E – Normal: Motor and sensory function normal



surface



flaccid



Paraplegia

Herrn JALLABERT,

Professors der Experimental-Philosophie und
Mathematik, Mitglieds der Königl. Gesellschaften der
Wissenschaften zu London und Montpellier, wie
auch der Academie des Institut Bononiens.

EXPERIMENTA
ELECTRICA
USIBUS MEDICIS APPLICATA.

Oder

Versuche

über die

Electricität,

aus denen der herrliche Nutzen derselben
in der

Orthocynwissenschaft

und insbesondere in der Kur eines Lähmen
zu ersehen,

nebst einigen Vermuthungen über die Ursache

der Wirkungen der Electricität.

Denn zu Ende beigefügt

Herrn de SAUVAGES

Königl. Rath und Professors zu Montpellier &c.

Sendschreiben,

an Herrn D. BRUHIER,

von den Versuchen so an einigen Lähmen un-
ter seiner Aufsicht gemacht worden.

Aus dem Französischen übersezt.

WILHELM, bey Johann Rudolf Zim Hof,
1750.



Nachricht

des Herausgebers der Pariser
Ausgabe.

296

) ()

von Montpellier erhalten, hier beifüge.
Es scheint derselbe sehr tauglich zu seyn,
zu Anstellung neuer Versuchen aufzu-
muntern, und man kan hoffen, daß die
Electricität für Krankheiten die die
Arzneymissenschaft bisher nur mit sehr
schwächtigen Waffen angriffe, ein
sehr kräftiges Mittel werden
könne.





Vienna FES Workshop

since 1983



14th Vienna International Workshop on Functional Electrical Stimulation

Sep 27 - 30, 2022 | Innsbruck, Austria

<https://fesworkshop.org/14th-workshop-2022>



Smile and Breathe: Atmung, Schlucken, Mimik – Chancen und Herausforderungen der Behandlung mittels Funktioneller Elektrostimulation

18. & 19. November 2022 im International FES Centre®, Nottwil und online via Zoom

Ziel des Kurses ist das Erlernen von theoretischen und praktischen Grundlagen der Behandlung mittels Funktioneller Elektrostimulation in der Neurorehabilitation bei Störungen der Atmung, des Schluckens und der Mimik.

<https://www.paraplegie.ch/spz/de/kurs-atmung-schlucken-mimik-international-fes-centrer/>